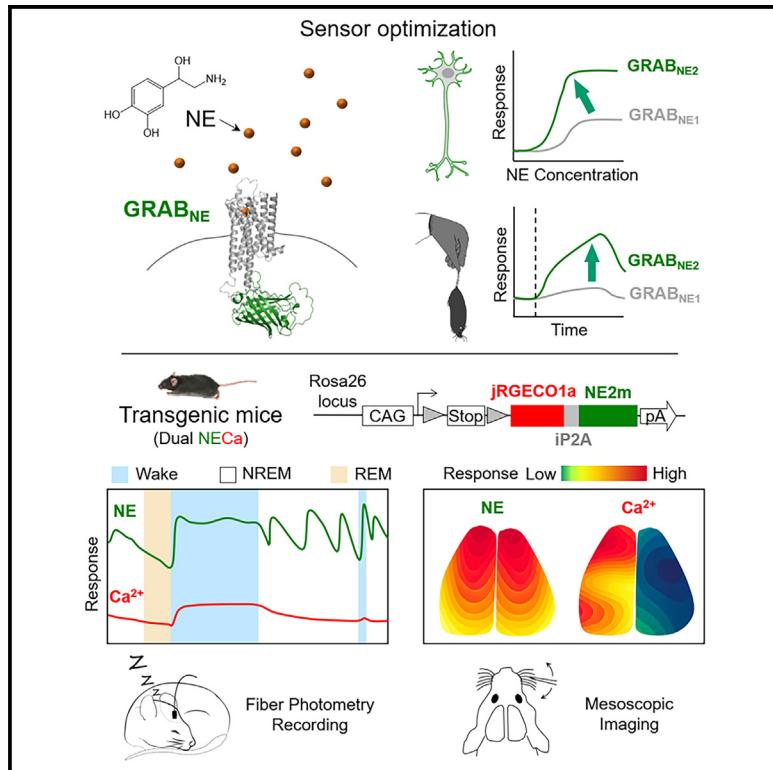


Monitoring norepinephrine release *in vivo* using next-generation GRAB_{NE} sensors

Graphical abstract



Authors

Jiesi Feng, Hui Dong,
Juliet E. Lischinsky, ..., Guohong Cui,
Dayu Lin, Yulong Li

Correspondence

jiesifeng@pku.edu.cn (J.F.),
yulongli@pku.edu.cn (Y.L.)

In brief

Feng et al. optimized a pair of GRAB_{NE} sensors with enhanced norepinephrine (NE) sensitivity both *in vitro* and *in vivo*. They also developed a Cre-dependent knockin transgenic mouse line for cell-type-specific dual-color imaging of NE and calcium, unveiling distinct neuromodulation dynamics across physiological states.

Highlights

- Improved GRAB_{NE} sensors offer enhanced NE sensitivity both *in vitro* and *in vivo*
- GRAB_{NE2m} and GRAB_{NE2h} expand the dynamic range of NE detection
- New KI mouse line enables consistent and concurrent NE and calcium recordings
- NE and calcium dynamics show distinct patterns in various physiological states



NeuroResource

Monitoring norepinephrine release *in vivo* using next-generation GRAB_{NE} sensors

Jiesi Feng,^{1,2,3,*} Hui Dong,^{1,2,3} Julieta E. Lischinsky,⁴ Jingheng Zhou,⁵ Fei Deng,^{1,2} Chaowei Zhuang,⁶ Xiaolei Miao,^{1,2,7} Huan Wang,^{1,2} Guochuan Li,¹ Ruyi Cai,¹ Hao Xie,⁶ Guohong Cui,⁵ Dayu Lin,⁴ and Yulong Li^{1,2,3,8,9,10,11,*}

¹State Key Laboratory of Membrane Biology, School of Life Sciences, Peking University, Beijing 100871, China

²PKU-IDG/McGovern Institute for Brain Research, Beijing 100871, China

³Peking-Tsinghua Center for Life Sciences, New Cornerstone Science Laboratory, Academy for Advanced Interdisciplinary Studies, Peking University, Beijing 100871, China

⁴Neuroscience Institute, New York University School of Medicine, New York, NY 10016, USA

⁵Neurobiology Laboratory, National Institute of Environmental Health Sciences, National Institutes of Health, Research Triangle Park, NC 27709, USA

⁶Department of Automation, Tsinghua University, Beijing 100084, China

⁷Department of Anesthesiology, Beijing Chaoyang Hospital, Capital Medical University, 100020 Beijing, China

⁸Chinese Institute for Brain Research, Beijing 102206, China

⁹Institute of Molecular Physiology, Shenzhen Bay Laboratory, Shenzhen, Guangdong 518055, China

¹⁰National Biomedical Imaging Center, Peking University, Beijing 100871, China

¹¹Lead contact

*Correspondence: jiesifeng@pku.edu.cn (J.F.), yulongli@pku.edu.cn (Y.L.)

<https://doi.org/10.1016/j.neuron.2024.03.001>

SUMMARY

Norepinephrine (NE) is an essential biogenic monoamine neurotransmitter. The first-generation NE sensor makes *in vivo*, real-time, cell-type-specific and region-specific NE detection possible, but its low NE sensitivity limits its utility. Here, we developed the second-generation GPCR-activation-based NE sensors (GRAB_{NE2m} and GRAB_{NE2h}) with a superior response and high sensitivity and selectivity to NE both *in vitro* and *in vivo*. Notably, these sensors can detect NE release triggered by either optogenetic or behavioral stimuli in freely moving mice, producing robust signals in the locus caeruleus and hypothalamus. With the development of a novel transgenic mouse line, we recorded both NE release and calcium dynamics with dual-color fiber photometry throughout the sleep-wake cycle; moreover, dual-color mesoscopic imaging revealed cell-type-specific spatiotemporal dynamics of NE and calcium during sensory processing and locomotion. Thus, these new GRAB_{NE} sensors are valuable tools for monitoring the precise spatiotemporal release of NE *in vivo*, providing new insights into the physiological and pathophysiological roles of NE.

INTRODUCTION

Norepinephrine (NE) is a monoamine neurotransmitter that plays essential roles in both the central and peripheral nervous systems, including regulating the sleep-wake cycle,¹ the stress response,² attention,³ sensory processing,⁴ heart rate,⁵ and blood pressure.⁶ Previous methods for measuring NE release *in vivo* relied on either specific—but slow—microdialysis coupled with biomedical identification^{7–12} or rapid—but less specific—electrochemical methods,^{13–16} such as fast-scan cyclic voltammetry. The development of cell-based neurotransmitter fluorescent engineered receptors (CNiFERs)¹⁷ and fluorescence resonance energy transfer (FRET)-based sensors^{18–20} provided a means to optically measure NE release with high specificity and temporal resolution; however, the use of these tools has been limited by their undesirable immu-

nogenicity, relatively poor cell-type specificity, and/or narrow dynamic range.

We previously developed a set of genetically encoded G-protein-coupled receptor (GPCR)-activation-based (GRAB) NE sensors called GRAB_{NE1m} and GRAB_{NE1h} in which the NE-induced conformational change in the $\alpha 2$ adrenergic receptor ($\alpha 2$ AR) noradrenergic receptor drives a fluorescence change in circular permuted EGFP (cpEGFP).²¹ These fluorescent sensors outperformed the above traditional methods in sensitivity, selectivity, spatiotemporal resolution, and non-invasiveness. However, the first generation of GRAB_{NE} sensors, GRAB_{NE1m} and GRAB_{NE1h}, still had limitations on either molecular sensitivity or selectivity for NE. To overcome these limitations, we developed next-generation NE sensors, namely GRAB_{NE2m} and GRAB_{NE2h}, which show a 4-fold maximum fluorescence response, nanomolar affinity, and better ability to distinguish NE from dopamine



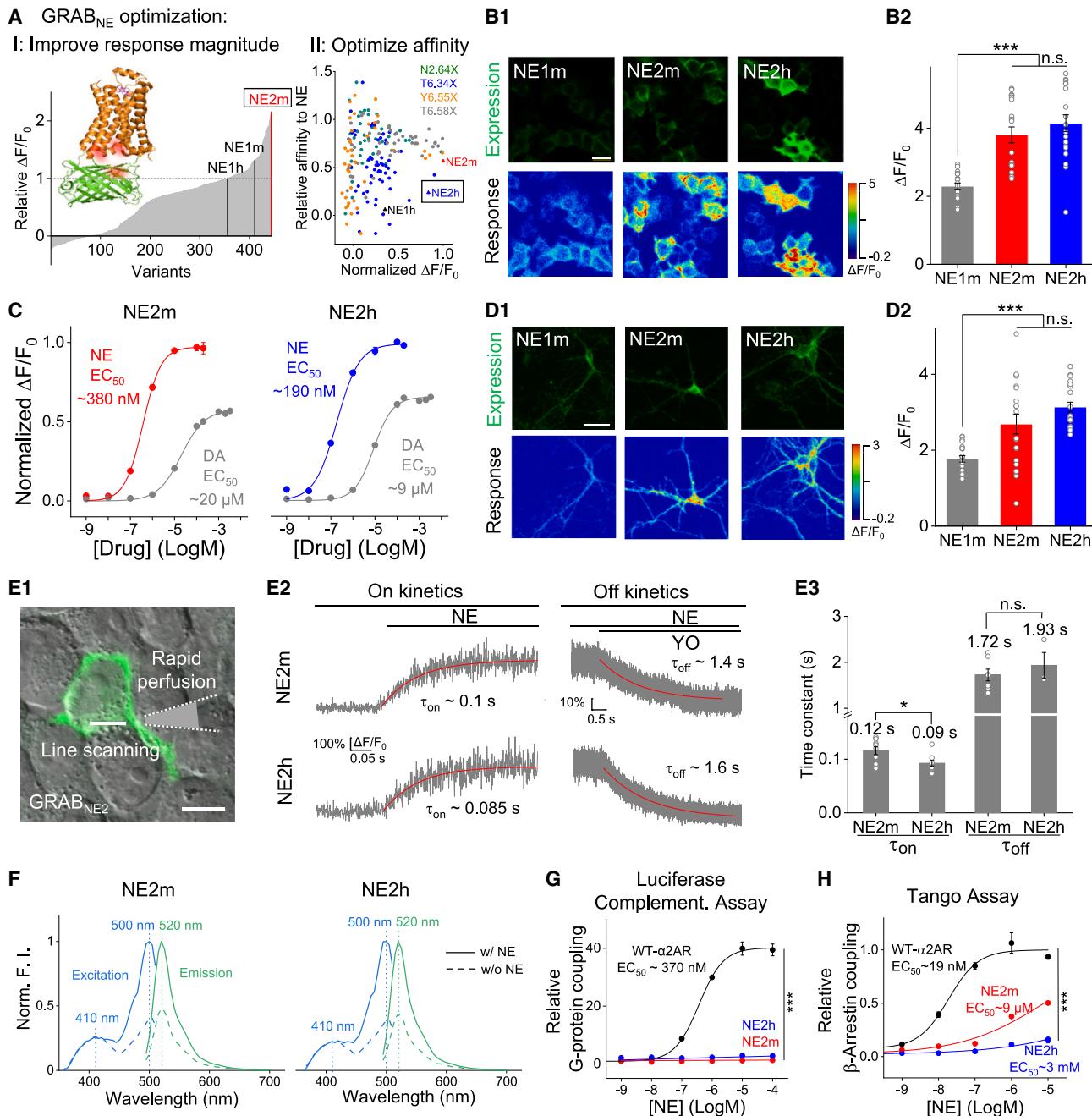


Figure 1. Optimization and *in vitro* characterization of next-generation GRAB_{NE} sensors

(A) (I) Optimization of GRAB_{NE} sensors by introducing random mutations at the interface between α 2AR and cpEGFP. The first-generation GRAB_{NE1m} and GRAB_{NE1h} sensors, as well as the next-generation GRAB_{NE2m} sensor, are indicated. (II) Further optimization to yield GRAB_{NE} sensors with increased ligand affinity, with relative ligand affinity plotted against $\Delta F/F_0$ (normalized to GRAB_{NE2h}). The various mutations are indicated, as well as GRAB_{NE1h}, GRAB_{NE2m}, and GRAB_{NE2h} sensors.

(B) (B1) Images of cultured HEK293T cells expressing GRAB_{NE1m}, GRAB_{NE2m}, or GRAB_{NE2h}. The top row shows baseline fluorescence, while the bottom row shows the change in fluorescence ($\Delta F/F_0$) in response to 100 μ M NE. (B2) Summary of $\Delta F/F_0$; $n = 20$ cells from 3 cultures per group.

(C) Normalized dose-response curves for GRAB_{NE2m} (left) and GRAB_{NE2h} (right) in response to NE and DA, respectively, in cultured HEK293T cells. The corresponding EC_{50} values of NE and DA are indicated. E_{max}/EC_{50} difference between NE and DA for GRAB_{NE2m} and GRAB_{NE2h} is 94- and 73-fold, respectively. $n = 3$ independent cultures each.

(D) Same as (B), except the sensors were expressed in cultured cortical neurons; $n = 20$ neurons from 3 cultures per group.

(E) The on and off kinetics of the change in fluorescence were measured using high-speed line scan imaging of HEK293T cells expressing GRAB_{NE2m} or GRAB_{NE2h}; τ_{on} was measured by fitting the rise in fluorescence upon rapid application of NE, and τ_{off} was measured by fitting the fluorescence decay upon

(legend continued on next page)

(DA). Importantly, these new sensors have rapid kinetics and negligible downstream coupling; in addition, when expressed *in vivo*, they produce an up to 5-fold stronger signal in response to optogenetically and behaviorally stimulated NE release compared with the previous GRAB_{NE} sensors. Moreover, we generated a Cre-dependent transgenic mouse line expressing both green fluorescent GRAB_{NE2m} and the red fluorescent calcium indicator jRGECO1a,²² which we then used to simultaneously monitor cell-type-specific NE release and calcium dynamics during the sleep-wake cycle, sensory processing, and locomotion. Together, these robust new tools can be used to measure noradrenergic activity under a wide range of physiological and pathophysiological conditions, providing important new insights into the functional role of NE in both health and disease.

RESULTS

Optimization and *in vitro* characterization of next-generation GRAB_{NE} sensors

Our previous fluorescent NE sensors GRAB_{NE1m} and GRAB_{NE1h} reported endogenous NE release with high spatio-temporal resolution²¹; however, when used *in vivo*, these sensors have a relatively modest change in fluorescence (~5% in response to optogenetic stimulation in the locus coeruleus [LC]), possibly due to low NE sensitivity. GRAB sensors respond to ligand binding by transducing the receptor's conformational change into a change in cpEGFP fluorescence. To increase the sensitivity of our GRAB_{NE} sensors, we systematically performed site-directed mutagenesis of around 20 amino acids (Figure S1) in GPCR backbone and cpEGFP of GRAB_{NE1h} and then screened the fluorescence responses of more than 400 candidate sensors in HEK293T cells using a high-content imaging system. Among these candidates, one sensor, GRAB_{NE2m}, produced the highest change in fluorescence ($\Delta F/F_0$) in response to NE (Figure 1A). To further increase the sensor's affinity, we screened sites related to ligand binding and identified a high-affinity sensor, which we call GRAB_{NE2h} (Figures 1A and S1).

Next, we expressed the first-generation GRAB_{NE1m} sensor and our second-generation GRAB_{NE2m} and GRAB_{NE2h} sensors in HEK293T cells (Figures 1B and S2A) and found that applying 100 μ M NE induced a peak $\Delta F/F_0$ of 230% \pm 9%, 381% \pm 23%, and 415% \pm 25%, respectively (Figure 1B2). In addition to their stronger response to NE, both GRAB_{NE2m} and GRAB_{NE2h} had good membrane trafficking comparable to membrane-targeted EGFP (Figure S2A). Furthermore, both GRAB_{NE2m} and GRAB_{NE2h} retained the ligand selectivity of the parent α 2AR receptor, responding to epinephrine (Epi) with a

similar EC₅₀ to NE (Figure S2B), but did not respond to trace amines and major NE metabolites, including octopamine (OA), tyramine (TA), phenethylamine (PEA), vanillylmandelic acid (VMA), normetanephrine (NMN), and 3-methoxy-4-hydroxyphenylglycol (MHPG) in full doses (Figure S2C). Consistently, NE sensors do not respond to other neurochemicals, including the β 2-adrenergic receptor agonist isoprenaline (ISO), acetylcholine (ACh), serotonin (5-HT), glutamate (Glu), γ -aminobutyric acid (GABA), adenosine (Ado), or histamine (HA); finally, the NE-induced response was blocked by the α 2AR antagonist yohimbine (YO) but not the β 2AR antagonist ICI-118,551 (ICI) (Figure S2D). To test the selectivity between NE and DA, which share very similar chemical structures, we performed dose-response curves for GRAB_{NE2m} and GRAB_{NE2h} and measured apparent affinity values of 380 and 190 nM, respectively (with 2- to 5-fold increase compared with GRAB_{NE1m}), in response to NE, with significantly lower affinity for DA (20 and 9 μ M, respectively) (Figure 1C). Notably, the maximum response induced by high-concentration DA is only 60%–65% of that induced by NE. Thus, we introduced a parameter E_{max}/EC_{50} ²³ to better evaluate the selectivity between ligands, taking both the efficacy (E_{max}) and potency (EC_{50}) into consideration. We found that the E_{max}/EC_{50} difference between NE and DA is 37-fold for the prototype GRAB_{NE1h} while 94-fold and 73-fold for GRAB_{NE2m} and GRAB_{NE2h}, respectively, which demonstrated an improved selectivity for the next-generation NE sensors. To test the performance of our GRAB_{NE} sensors in neurons, we expressed GRAB_{NE2m} and GRAB_{NE2h} in cultured cortical neurons (Figures 1D and S2A). Both sensors' membrane trafficking and peak $\Delta F/F_0$ were consistent with our results obtained using HEK293T cells.

To determine whether the next-generation GRAB_{NE} sensors respond to NE with rapid kinetics, we locally puffed a saturating concentration of 10 μ M NE onto HEK293T cells expressing either GRAB_{NE2m} or GRAB_{NE2h} and measured the change in fluorescence using high-speed line scan imaging (Figure 1E1). Fitting the rising phase of the fluorescence change using a single exponential function yielded average τ_{on} values of 0.12 and 0.09 s for GRAB_{NE2m} and GRAB_{NE2h}, respectively (Figure 1E). We also fit the decrease in fluorescence following the addition of YO in the presence of NE and obtained average τ_{off} values of 1.72 and 1.93 s for GRAB_{NE2m} and GRAB_{NE2h}, respectively. The kinetics of GRAB_{NE2m} and GRAB_{NE2h} is a bit slower than GRAB_{NE1m},²¹ possibly due to the higher affinity.

Next, we measured the spectral properties of GRAB_{NE2m} and GRAB_{NE2h} using one-photon excitation. We found that both sensors have excitation peaks at 410 and 500 nm and an emission peak at 520 nm (Figure 1F), similar to the spectra of GFP and

application of the α 2AR antagonist yohimbine (YO) in the continued presence of NE. (E1) shows the experimental setup, including the line-scanning region and the pipette for rapid drug application. (E2) and (E3) show representative traces and the summary data, respectively; $n \geq 3$ cells from 3 cultures per group. (F) Excitation (blue) and emission (green) spectra of GRAB_{NE2m} (left) and GRAB_{NE2h} (right) in the absence (dashed lines) and presence (solid lines) of 100 μ M NE using one-photon imaging.

(G) Summary of relative dose-dependent downstream G protein coupling of the wild-type α 2 adrenergic receptor (WT- α 2AR), GRAB_{NE2m}, and GRAB_{NE2h} expressed in HEK293T cells measured using the luciferase complementation mini-G protein assay. $n = 3$ wells with $\geq 10^5$ cells each.

(H) Summary of relative dose-dependent downstream β -arrestin coupling of WT- α 2AR, GRAB_{NE2m}, and GRAB_{NE2h} expressed in HTLA cells measured using the Tango assay. $n = 3$ wells with $\geq 10^5$ cells each.

The scale bars in (B) and (E) represent 20 μ m; the scale bar in (D) represents 50 μ m. Unless noted, summary data are presented as the mean \pm SEM. ***p < 0.001, *p < 0.05, and n.s., not significant (Student's t test and two-way ANOVA). See also Figures S1 and S2.

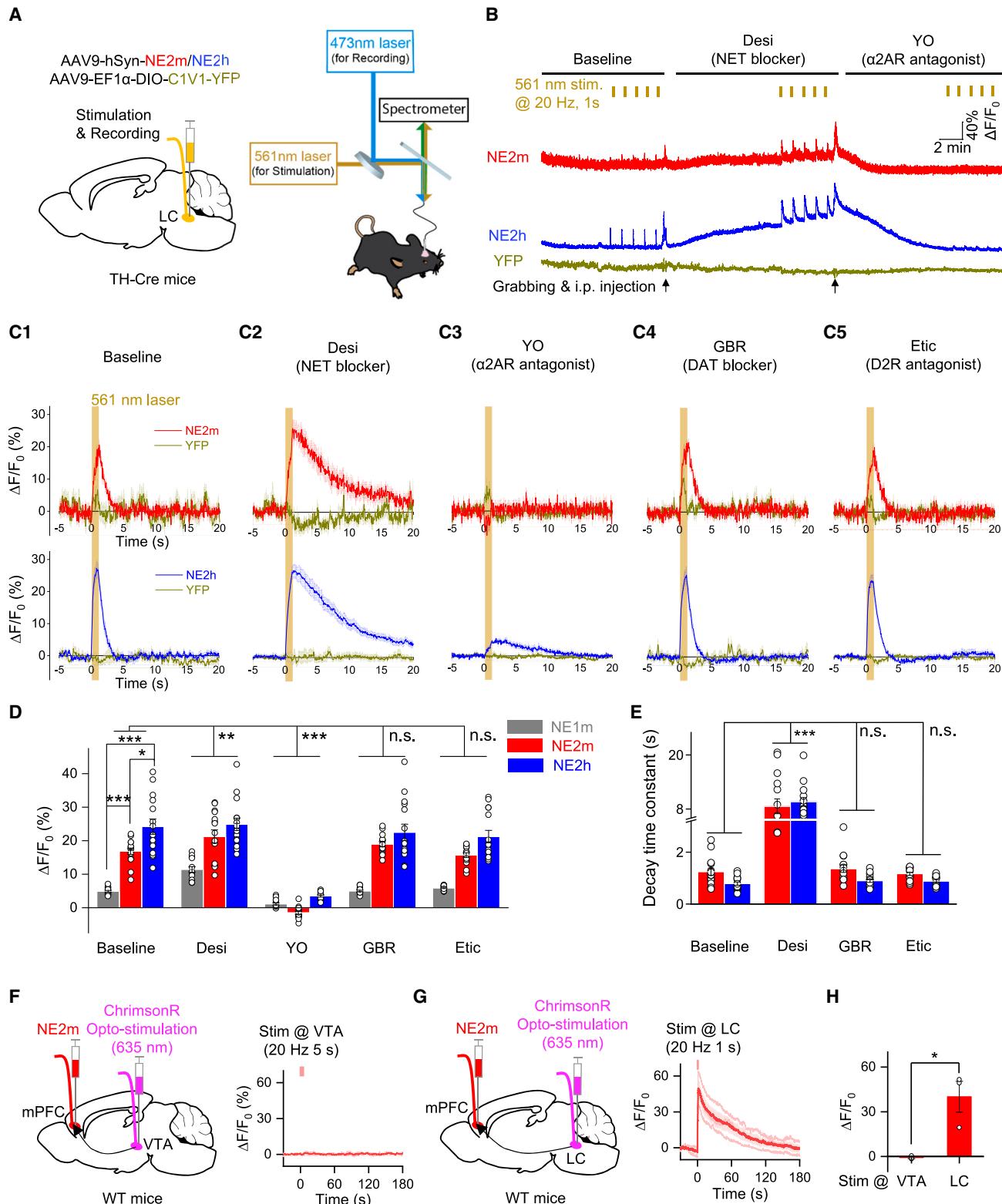


Figure 2. Detection of optogenetically evoked NE release in freely moving mice

(A) Experimental design depicting the strategy for expressing GRAB_{NE2m} and GRAB_{NE2h} and recording the change in fluorescence in response to optical stimulation of C1V1 in the locus coeruleus (LC).

(legend continued on next page)

the calcium indicator GCaMP; thus, our sensors are compatible with various established imaging systems.

Because overexpressed GPCRs or their derivatives may induce downstream signaling, they have the potential to affect cellular physiology and may, therefore, be unsuitable for use in *in vivo* imaging. To rule out this possibility, we examined whether GRAB_{NE2m} and GRAB_{NE2h} induce downstream G protein and/or β -arrestin signaling using a luciferase complementation mini-G protein assay and the Tango assay, respectively (see **STAR Methods**). We found that both sensors have negligible downstream coupling (Figures 1G and 1H), suggesting that overexpressing either GRAB_{NE2m} or GRAB_{NE2h} does not significantly affect cellular physiology. In addition, GRAB_{NE} sensor expression does not alter the dose-dependent G protein and β -arrestin signaling of native wild-type (WT) α 2AR (Figure S2E), suggesting the minimal impact of GRAB_{NE} sensors on the function of native receptors.

Detection of optogenetically evoked NE release in freely moving mice

Having shown that our next-generation GRAB_{NE} sensors have superior sensitivity, high specificity, rapid kinetics, and negligible downstream coupling *in vitro*, we then examined whether these sensors can report endogenous NE release *in vivo* when expressed in the LC of TH-Cre mice together with the optogenetic actuator C1V1 linked to YFP (Figure 2A). For this experiment, we used spectrally resolved fiber photometry²⁴ to measure GRAB_{NE} and YFP simultaneously. We found that optogenetic stimulation of LC-NE neurons elicited increases in GRAB_{NE2m} and GRAB_{NE2h} fluorescence in freely moving mice but did not affect YFP fluorescence (Figures 2B and 2C1). In addition, an intraperitoneal (i.p.) injection of the NE transporter (NET) inhibitor desipramine (Desi) caused a progressive increase in the basal fluorescence of GRAB_{NE2h}, reflecting an accumulation of extracellular NE and the high affinity of GRAB_{NE2h} for NE (Figure 2B); moreover, in the presence of Desi, the response induced by optogenetic stimulation was larger in magnitude and had slower decay kinetics (Figure 2C2). Conversely, an i.p. injection of the α 2AR antagonist YO nearly abolished both the Desi-induced increase in basal fluorescence and the optogenetic-stimulation-evoked increase in GRAB_{NE2m} and GRAB_{NE2h} fluorescence (Figures 2B and 2C3). In separate experiments, we injected the mice with either the selective DA transporter (DAT) inhibitor GBR-12909 followed by the D2R-specific antagonist eticlopride (Etic), which had no effect on basal fluorescence (data not shown) or the kinetics or magnitude of the optogenetically stimulated increase in GRAB_{NE2m} and GRAB_{NE2h} fluores-

cence (Figures 2C–2E). Importantly, we found that GRAB_{NE2m} and GRAB_{NE2h} had \sim 17% and 24% increase in $\Delta F/F_0$, respectively, in response to a single train of light pulses (Figure 2D), a 2.4- to 3.9-fold improvement over the first-generation GRAB_{NE1m} sensor. These results suggest that our next-generation GRAB_{NE} sensors can reliably detect optogenetically evoked NE release in the LC of freely moving mice.

To further test the utility of GRAB_{NE} sensors, we conducted fiber photometry recording in mouse medial prefrontal cortex (mPFC) expressing GRAB_{NE2m} during optogenetic activation of ventral tegmental area (VTA)—a brain region that sends dopaminergic projections to mPFC, or LC—a brain region that sends noradrenergic projections to mPFC. We found that 20-Hz, 1-s optogenetic stimulation of LC elicited a robust fluorescence increase in mPFC, while 20-Hz, 5-s optogenetic stimulation of VTA did not induce detectable fluorescence increases in mPFC (Figures 2F–2H). Taken together, GRAB_{NE2m} enables sensitive and specific measurements of NE release *in vivo*.

Next-generation NE sensors report behaviorally evoked NE release *in vivo* in response to stressful stimuli

The lateral hypothalamus (LH) is a target of the LC and has been shown to release NE during specific behaviors such as stress.²¹ We therefore examined whether our next-generation GRAB_{NE} sensors can exhibit higher signals in measuring behaviorally evoked NE release in the LH of freely moving mice. We expressed GRAB_{NE1m}, GRAB_{NE2m}, or GRAB_{NE2h} in the LH of WT mice (Figure 3A and 3B) and then performed fiber photometry recordings during stress-inducing activities, including tail suspension (Figure 3C), forced swimming (Figure 3D), and hand presentation (Figure 3E). Consistent with previous reports,²¹ all three stressors increased GRAB_{NE} fluorescence. Moreover, both GRAB_{NE2m} and GRAB_{NE2h} had a larger response (up to 3.7-fold) during tail suspension than GRAB_{NE1m} (Figure 3C). Interestingly, GRAB_{NE2h} had the largest response among all three sensors during both forced swimming and hand presentation (Figures 3C and 3E). In addition, an i.p. injection of the selective NET inhibitor atomoxetine (ATX) induced a slow decay in the response to tail suspension without significantly affecting peak $\Delta F/F_0$; in contrast, the α 2AR antagonist YO significantly reduced the tail suspension-evoked increase in GRAB_{NE2m} and GRAB_{NE2h} fluorescence (Figures 3F1 and 3G1). Finally, neither the selective DAT blocker GBR-12909 nor the D2R antagonist sulpiride affected the magnitude or kinetics of the response (Figures 3F2 and 3G2). These results indicate that our next-generation GRAB_{NE} sensors can be used to monitor the release of endogenous NE in response to stress.

(B) Representative traces of optogenetically stimulated fluorescence change in GRAB_{NE2m} (red), GRAB_{NE2h} (blue), and YFP (olive, as a negative control) in the LC before (baseline, left), after an i.p. injection of the NE transporter (NET) blocker desipramine (Desi, 10 mg/kg, middle), and after an i.p. injection of the α 2AR antagonist yohimbine (YO, 2 mg/kg, right). The vertical tick marks (yellow) indicate the optogenetic stimuli delivered at 20 Hz.

(C–E) Average traces (C), summary of $\Delta F/F_0$ (D), and summary of decay time constants (E) of the change in fluorescence of GRAB_{NE2m} (top row in C, red) and GRAB_{NE2h} (bottom row in C, blue) in response to optical stimulation in the LC following treatment with the indicated compounds. Also shown in (C) are the fluorescence traces for YFP. The data for GRAB_{NE1m} in (D) and (E) were reproduced²¹ for comparison. n = 15 trials in 3 mice per group. GBR, GBR-12909; Etic, eticlopride.

(F–H) Fiber photometry recording of GRAB_{NE2m} fluorescence in mPFC reports specific NE dynamics during optogenetic stimulation of VTA (F) and LC (G). Summary data (H) of GRAB_{NE2m} peak responses during optogenetic stimulation on VTA and LC. n = 3 mice each.

Unless noted, summary data are presented as the mean \pm SEM. ***p < 0.001, **p < 0.01, *p < 0.05, and n.s., not significant (two-way ANOVA for D and E, Student's t test for H).

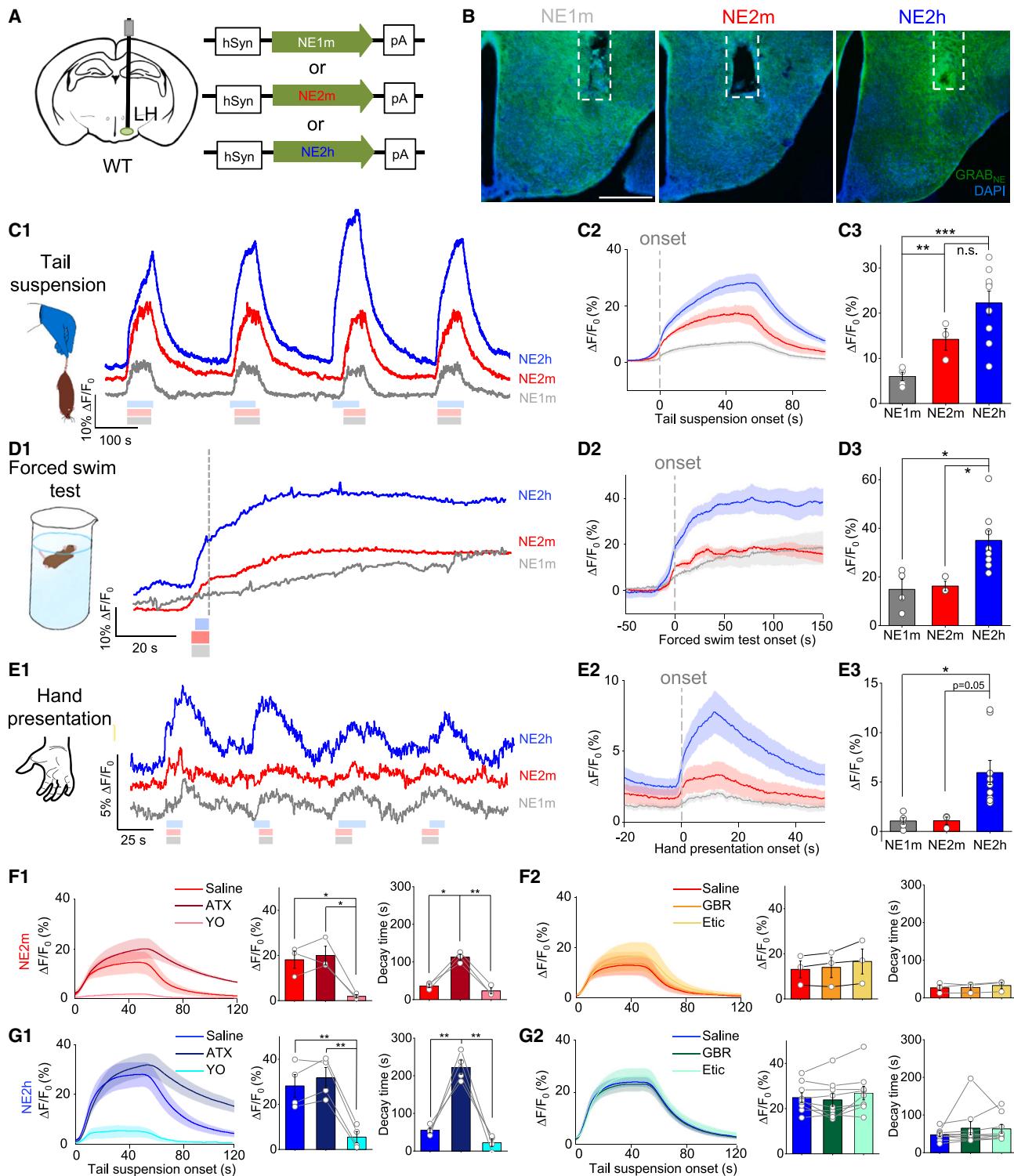


Figure 3. Next-generation NE sensors report behaviorally evoked NE release *in vivo* in response to stressful stimuli

(A) Schematic diagram depicting the strategy for virus injection, fiber placement, and the recording site for GRAB_{NE1m}, GRAB_{NE2m}, or GRAB_{NE2h} in the lateral hypothalamus (LH).

(B) Fluorescence images of brain sections of mice injected with virus expressing the indicated GRAB_{NE} sensors (green); the nuclei were counterstained with DAPI (blue). The position of the fiber is indicated by dashed white rectangles. The scale bar, 500 μm.

(legend continued on next page)

NE and calcium dynamics during the sleep-wake cycle

Genetically encoded GRAB_{NE} sensors can also be used to examine the spatiotemporal dynamics of NE release in the brain, which is a tightly regulated, complex process that can depend on a variety of factors, such as the state of arousal and the activation of distinct brain regions. Moreover, previous studies suggested that specific brain regions may have either similar or distinct patterns of neurotransmitter release during the sleep-wake cycle.^{25–27} To measure the dynamics of NE release in specific brain regions and determine whether this release is synchronized between brain regions, we virally expressed GRAB_{NE2m} to simultaneously monitor NE levels in both the mPFC and the preoptic area of the hypothalamus (POA) (Figure 4A), two brain regions critically involved in regulating arousal and wakefulness. Meanwhile, we used electroencephalogram (EEG) and electromyogram (EMG) recordings to determine the animal's sleep-wake state—i.e., awake, in non-rapid eye movement (NREM) sleep, or in rapid eye movement (REM) sleep. Dual-site continuous fiber photometry recording revealed that the changes in NE levels were closely synchronized between the mPFC and POA throughout the sleep-wake cycle (Figures 4B–4D). Specifically, consistent with previous results,^{25,26} NE levels were relatively high during wakefulness and NREM sleep but low during REM sleep (Figure 4C). To analyze NE kinetics during the various state transitions, we calculated the t_{50} from each fluorescence trace and found similar kinetics between the mPFC and POA, with a rapid increase in NE release during the transition from REM sleep to the awake state (~5 s) and from NREM sleep to the awake state (~4 s), suggesting rapid NE release during arousal (Figures 4E and 4F). In contrast, the decrease in NE release was relatively slow during the transition from the awake state to NREM sleep (~22 s) and from NREM sleep to REM sleep (~30 s).

Although using virus injection to express genetically encoded sensors has several advantages, this approach also has several practical limitations, including the need for invasive surgery to inject the virus, limited region of delivery, variable levels of expression, and potential long-term cytotoxicity. To overcome these limitations, we generated a transgenic mouse line that expresses floxed GRAB_{NE2m} and jRGECO1a²²—a red fluorescent calcium indicator—driven by the ubiquitous CAG promoter and targeted to the *Rosa26* locus.^{28–30} Upon Cre expression, the cells in these mice express both GRAB_{NE2m} and jRGECO1a; these mice are referred to hereafter as dual-NECa mice (Figure 4G).

First, we virally expressed Cre in the mPFC of dual-NECa mice and used dual-color fiber photometry recording to measure both NE and calcium while monitoring the sleep-wake state using EEG and EMG (Figure 4H). We found that the GRAB_{NE2m} sensor expressed in the mPFC of our dual-NECa mice faithfully reported

NE release throughout the sleep-wake cycle, consistent with previous reports.^{25,26} In addition, by measuring jRGECO1a fluorescence, we observed relatively higher noradrenergic and calcium activities during the awake state, low noradrenergic and calcium activities during REM sleep, and distinct patterns of oscillatory NE release and relatively low calcium activity during NREM sleep (Figures 4I, 4J, and S3B–S3D).

Importantly, neither the amplitude nor the kinetics of the NE signals measured in the dual-NECa transgenic mice differed significantly from those measured in mPFC neurons expressing GRAB_{NE2m} via adeno-associated virus (AAV)-mediated delivery (Figures 4I–4K). Furthermore, the NE signals recorded in the dual-NECa mice had lower within-group variation than that of viral expression (Figure 4L). Taken together, these findings indicate that our dual-NECa transgenic mouse line is a useful tool to consistently report NE release and calcium dynamics simultaneously with temporal precision.

Mesoscopic NE and calcium dynamics in the dorsal cortex of awake mice

Another advantage of our dual-NECa mouse is that it can be crossed with established Cre-driver lines to express both GRAB_{NE2m} and jRGECO1a in specific cell types. Approximately 500 Cre-driver lines expressing reporter genes globally or in specific cell types and/or tissues are available from the Jackson Laboratory. We first crossed our dual-NECa reporter mouse with the CaMKIIα-Cre mouse (Figure 5A, top) to measure NE release and calcium dynamics specifically in excitatory neurons. The heterozygous mouse strain displays a healthy phenotype with no significant abnormalities or defects in growth, behavior, and reproduction (Figure S3A). Noradrenergic neurons in the LC, which project to the entire brain and modulate a wide range of behaviors, including attention, stress, and cognition, have been reported to have high molecular and functional heterogeneity^{31,32}; thus, the pattern of NE release during these behaviors has remained poorly understood. Based on the one-photon spectra of GRAB_{NE2m} and jRGECO1a (Figure 5A, bottom), we performed cortex-wide two-channel imaging mesoscopy using 488- and 561-nm lasers to excite GRAB_{NE2m} and jRGECO1a, with an additional 405-nm laser signal used to correct for hemodynamic changes in the cortex³³ (Figure 5B; see STAR Methods).

To confirm that the change in fluorescence measured using dual-color mesoscopy was specific for NE, we applied auditory stimuli to mice expressing either GRAB_{NE2m} or our previously reported NE-insensitive mutant sensor, GRAB_{NEmut}.²¹ We applied a 1-s pulse of white noise as the auditory stimulus and measured green fluorescence through a 6-mm × 8-mm D-shaped cranial window; we also used an infrared camera to record pupil size to confirm the mouse's autonomic response to the auditory

(C–E) Representative traces (1), averaged per-stimulus histograms (2), and summary data (3) of GRAB_{NE} fluorescence ($\Delta F/F_0$) measured before, during, and after tail suspension (C), before and during forced swimming (D), and before, during, and after hand presentation (E); $n \geq 3$ animals per group. The shaded bars in (C)–(E) indicate hand presentation to deliver respective stimuli. The gray dashed lines in (C)–(E) indicate the onset of respective stimuli.

(F–G) Averaged per-stimulus histograms (left), summary data in GRAB_{NE} fluorescence ($\Delta F/F_0$) (middle), and post-test decay time (right) measured in mice expressing GRAB_{NE2m} (F) or GRAB_{NE2h} (G) in the LC during the tail suspension test 25 min after an i.p. injection of saline (Sal), atomoxetine (ATX), yohimbine (YO), GBR-12909 (GBR), or eticlopride (Etic) as indicated; $n \geq 3$ animals per group.

Unless noted, summary data are presented as the mean ± SEM. *** $p < 0.001$, ** $p < 0.01$, * $p < 0.05$, and n.s., not significant (Student's *t* test).

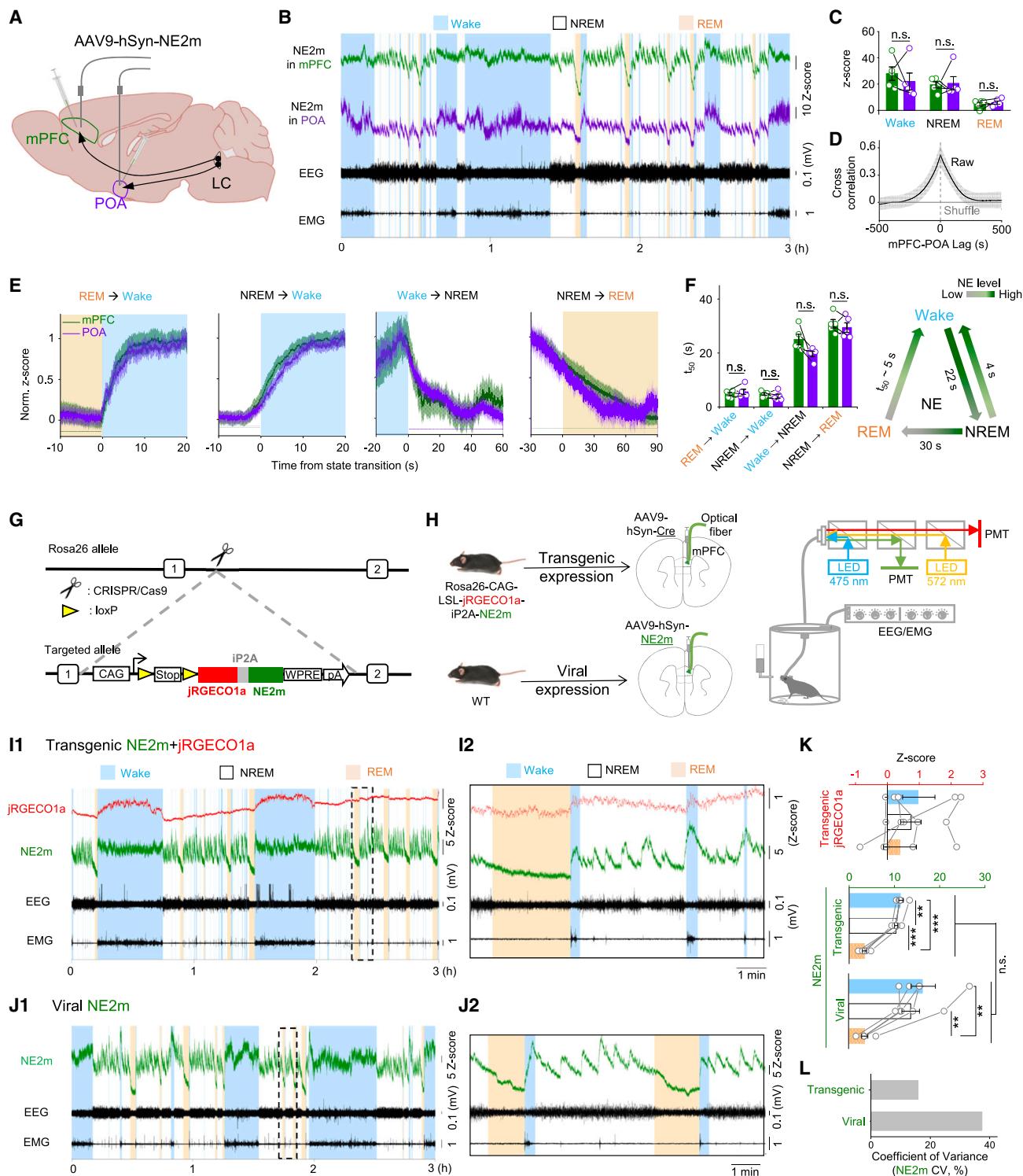


Figure 4. NE and calcium dynamics during the sleep-wake cycle

(A) Illustration depicting the strategy for virus injection and fiber placement for recording GRAB_{NE2m} fluorescence in both the medial prefrontal cortex (mPFC) and preoptic area of the hypothalamus (POA) during the sleep-wake cycle. The LC and its projections to the mPFC and POA are also indicated.

(B and C) Representative traces of the GRAB_{NE2m} fluorescence signal (expressed as a Z score), EEG, and EMG recordings (B) and summary data of GRAB_{NE2m} fluorescence measured in mPFC and POA during the wake state, NREM sleep, and REM sleep (C).

(legend continued on next page)

pulse (Figure 5C, top). We first verified that both GRAB_{NE2m} and GRAB_{NEmut} were expressed throughout the cerebral cortex (Figures 5C bottom and S4A). We then found that the application of the auditory pulse induced a time-locked increase in fluorescence in the mice expressing GRAB_{NE2m} but had no effect in mice expressing GRAB_{NEmut} (Figure 5D). In contrast, the auditory pulse caused an increase in pupil diameter in both groups, indicating the presence of a general arousal response (Figure S4B). In addition, the relatively homogeneous pattern of NE release in the cortex induced by the auditory stimulation (Figure 5D) is consistent with the reported distribution of LC fibers throughout the cortex.³⁵

Next, to measure cell-type-specific noradrenergic and calcium signaling in response to tactile stimuli, we crossed our dual-NECa mouse line with CaMKII α -Cre (with the mouse calcium/calmodulin-dependent protein kinase II alpha promoter driving Cre recombinase expression) or GFAP-Cre (with a mouse glial fibrillary acidic protein promoter sequence directing expression of Cre recombinase) lines to drive the expression of both GRAB_{NE2m} and jRGECO1a in excitatory neurons and astrocytes, respectively; we then performed mesoscopic imaging and measured the change in NE and calcium in response to unilateral whisker stimulation (Figure 5E). In the CaMKII α ::NECa mice, we observed a time-locked global increase in GRAB_{NE2m} fluorescence throughout the dorsal cortex, while the calcium signal increased only in the contralateral hemisphere, consistent with thalamocortical projections (Figure 5E). In addition, bilateral whisker stimulation induced a symmetrical concurrent increase in both NE and calcium (Figures 5F and S5A1). In contrast, we observed a similar global increase in GRAB_{NE2m} fluorescence in the GFAP::NECa mice but a relatively small and delayed calcium signal increase during both unilateral and bilateral whisker stimulation (Figures 5E, 5F, and S5A2).

As a further test of the effect of sensory stimuli on NE and calcium signaling in different cell types, we delivered either binocular or monocular visual stimuli to these mice. In the CaMKII α ::NECa mice, monocular visual stimulation induced an increase in calcium in the contralateral visual cortex (Figure S5C). Interestingly, however, binocular visual stimulation induced a small but measurable global increase in GRAB_{NE2m} fluorescence throughout the cortex, while monocular stimulation had no effect on either hemisphere. In contrast, visual stimulation did not affect either NE or calcium signaling in the GFAP::NECa mice (Figure S5B). Thus, dual-color mesoscopic imaging of our

dual-NECa transgenic mice revealed cell-type-specific differences in the spatiotemporal patterns of NE and calcium signaling in response to distinct sensory inputs, providing valuable insights into the underlying neural circuitry.

Finally, we examined NE and calcium signaling in response to spontaneous locomotor activity using the EMG data and the speed of the linear treadmill as a measure of the onset and duration of locomotion, respectively. In the CaMKII α ::NECa mice, we found that both the NE and calcium signals increased in the dorsal cortex with increased locomotor activity (Figure 5G1); similar results were obtained in the GFAP::NECa mice (Figure 5H1). We then aligned and averaged the peak response images of both the NE and calcium signals obtained from each mouse during locomotion and then segmented the dorsal cortex into distinct brain regions using the Allen Brain Atlas (Figures 5G2–5H3). We found that in both the CaMKII α ::NECa and GFAP::NECa mice, NE was released globally, with a high Spearman coefficient throughout the cortex (Figure 5I). In contrast, the calcium signal increased in the sensorimotor cortex in “hotspots” in the CaMKII α ::NECa mice, while the calcium signal increased globally in the GFAP::NECa mice with an ~2.8-s delay following the onset of locomotion (Figure 5J). These results shed new light on the intricate interplay between NE and calcium signaling in the brain during distinct behaviors.

DISCUSSION

Here, we developed the next-generation GRAB_{NE} sensors with increased response and sensitivity for NE. We then used these new sensors to detect optogenetically and behaviorally triggered NE release in the LC and LH of freely moving mice. In addition, we developed a novel transgenic mouse line expressing both GRAB_{NE2m} and the calcium sensor jRGECO1a in specific cell types and performed simultaneous dual-color recording and cell-type-specific spatiotemporal imaging of NE and calcium signaling during the sleep-wake cycle, sensory processing, and locomotion in behaving mice.

Given the structural similarity and widespread patterns of NE and DA throughout the brain, distinguishing these two monoamines is essential when performing *in vivo* behavioral studies. Moreover, because human noradrenergic receptors respond to both NE and DA, our goal is to increase the sensitivity of GRAB_{NE} sensors to NE while reducing their response to DA. Using cell-based screening, we identified specific combinations of

(D) Cross-correlation between GRAB_{NE2m} fluorescence measured in the mPFC and GRAB_{NE2m} fluorescence measured in the POA; also shown are the same raw data after being randomly shuffled.

(E) Representative time courses of the GRAB_{NE2m} fluorescence signal measured in the mPFC and POA during the indicated transitions between the indicated sleep-wake states.

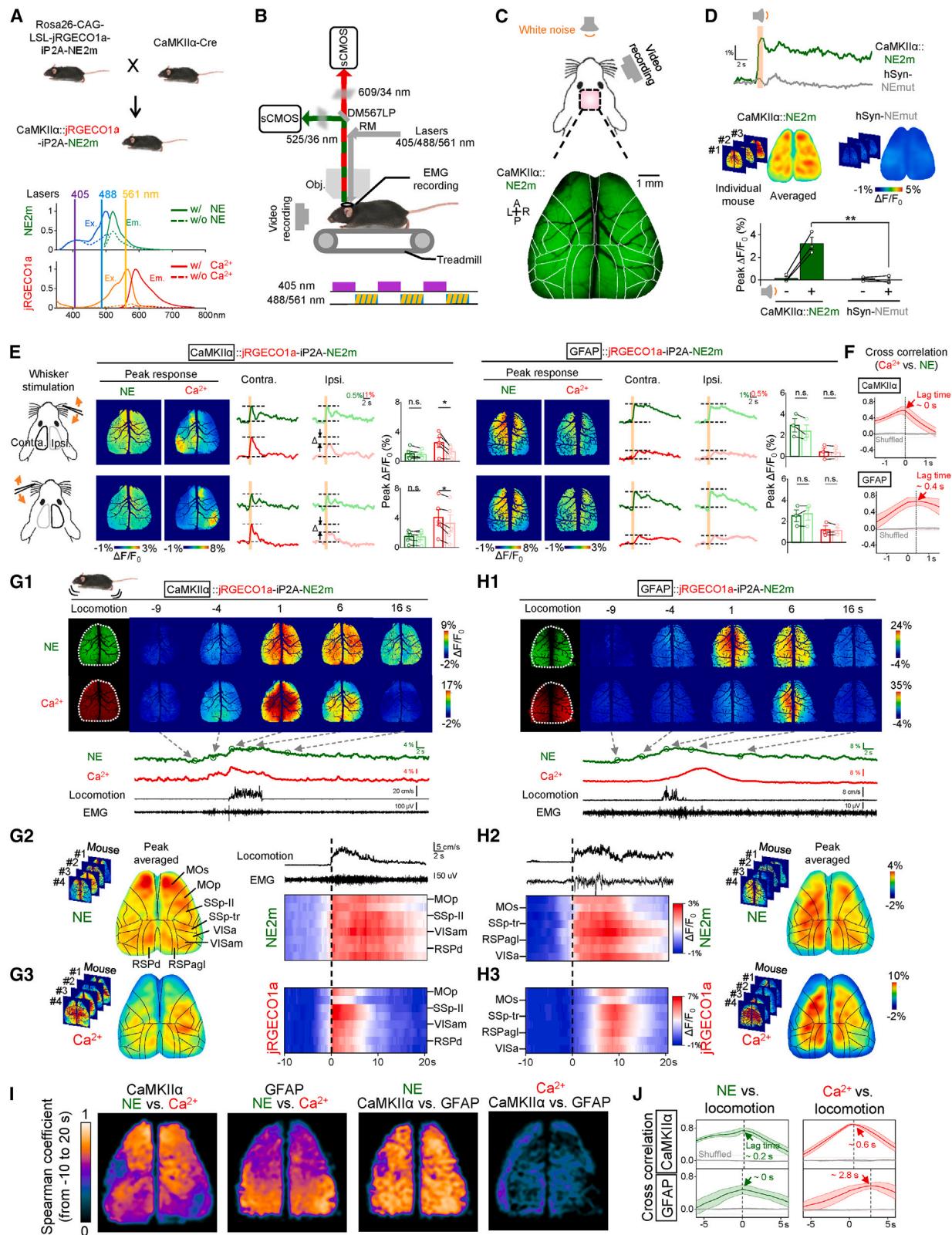
(F) Summary data (left) and summary model (right) of the t_{50} values measured for each transition between the indicated sleep-wake states.

(G) Strategy used to generate the cre-dependent transgenic knockin mouse line expressing both GRAB_{NE2m} and jRGECO1a in the Rosa26 locus (dual-NECa).

(H) Schematic illustration depicting the strategy used for virus injection and dual-color fiber photometry recording of GRAB_{NE2m} and jRGECO1a in the mPFC of dual-NECa transgenic mice (top) or wild-type (WT) mice (bottom) during the sleep-wake cycle.

(I–K) Representative jRGECO1a, GRAB_{NE2m}, EEG, and EMG traces (1), expanded traces (2) based on the dashed rectangle in (1), and summary (K) of the jRGECO1a and GRAB_{NE2m} signals measured in dual-NECa transgenic mice (I) or WT mice virally expressing GRAB_{NE2m} (J) during the awake state, NREM sleep, and REM sleep.

(L) Coefficient of variation (CV) between the transgenic GRAB_{NE2m} and virally expressed GRAB_{NE2m} signals measured during the sleep-wake cycle. $n = 5$ animals per group. Unless noted, summary data are presented as the mean \pm SEM. *** $p < 0.001$, ** $p < 0.01$, and n.s., not significant (two-way ANOVA for F, one-way ANOVA and Student's *t* test for K). See also Figure S3.



(legend on next page)

mutations that increased the sensors' sensitivity to NE without compromising their selectivity, suggesting the power of high-throughput screening in navigating complex chemical spaces. As a result, both GRAB_{NE2m} and GRAB_{NE2h} showed a high affinity to NE (380 and 190 nM, respectively), as well as an improved selectivity (E_{max}/EC_{50} difference) between NE and DA (94- and 73-fold, respectively) compared with GRAB_{NE1h}. Moreover, consistent with our *in vitro* results, our next-generation GRAB_{NE} sensors produce robust and specific *in vivo* signals in response to both optogenetic stimulation and behavioral events. A parallel green fluorescent GRAB NE sensor, namely nLightG,³⁶ showed better NE selectivity but lower affinity when compared with GRAB_{NE2m} and GRAB_{NE2h}. Since nLightG and GRAB_{NE} are based on different adrenergic receptors, α 1AR and α 2AR, respectively, they could be complementary tools when using additional pharmacology to modulate adrenergic systems.

It is worth highlighting that the fluorescence signals emitted by the GRAB_{NE2m} and GRAB_{NE2h} sensors do not vary with NE concentration, i.e., isosbestic, when the excitation light is within the range of 400–420 nm (Figure 1F). Thus, the commonly available 405-nm excitation light could be used as a control channel for *in vivo* experiments to distinguish fluorescence fluctuation caused by optic fiber bending and twisting during intense movements from signal changes due to NE release.

The newly generated dual-NECa transgenic mouse allows for the simultaneous monitoring of NE and calcium signaling in specific cell types and brain regions with a high spatiotemporal resolution during various physiological conditions and stimuli. Although the sensors' expression levels are presumably lower than AAV-mediated expression, the dual-NECa mice revealed similar changes in NE dynamics throughout the sleep-wake cycle, encompassing the signal amplitude and kinetics during state transitions. Moreover, a clear advantage of the dual-NECa mice is that the signals obtained have considerably lower within-group variance compared with viral expression, reflect-

ing the reliability and high replicability of using the dual-NECa mouse to image NE and calcium signaling. Furthermore, this transgenic mouse line can be used to express the NE and calcium sensors in virtually any cell type and/or tissue by crossing with specific Cre-reporter mice. We observed no detectable behavior abnormalities in the floxed transgenic mice or the floxed mice crossed with CaMKII α -Cre or GFAP-Cre mice in the open field test or the elevated plus maze test (Figure S3A). However, subtle behavior deficits may exist and require further investigation.

Finally, using dual-color mesoscopic imaging of dual-NECa mice, we observed global versus hotspot patterns of NE release and cell-type-specific calcium signaling during distinct sensory processing events and locomotion. Thus, integrating cortex-wide imaging with our dual-NECa reporter mice offers a unique opportunity to examine NE and calcium signaling on a large scale with both cell-type and molecular specificity in a wide range of physiological and pathophysiological contexts.

STAR★METHODS

Detailed methods are provided in the online version of this paper and include the following:

- **KEY RESOURCES TABLE**
- **RESOURCE AVAILABILITY**
 - Lead contact
 - Materials availability
 - Data and code availability
- **EXPERIMENTAL MODEL AND SUBJECT DETAILS**
 - Cell lines
 - Primary cell cultures
 - Animals
- **METHOD DETAILS**
 - Molecular cloning

Figure 5. Mesoscopic NE and calcium dynamics in dorsal cortex of awake mice

(A) (Top) Schematic diagram depicting the strategy for generating CaMKII α ::NECa mice by crossing dual-NECa mice with CaMKII α -Cre mice to drive the expression of GRAB_{NE2m} and jRGECO1a in excitatory neurons. (Bottom) One-photon excitation and emission spectra of GRAB_{NE2m} (in the absence and presence of ligand) and jRGECO1a²² (replotted from FPbase³⁴); the three excitation lasers used for mesoscopic imaging are also indicated.

(B) Schematic diagram depicting the dual-color mesoscopic imaging setup for recording GRAB_{NE2m} and jRGECO1a fluorescence in behaving mice. Excitation light alternated between green and red fluorescence imaging, and artifacts were corrected using 405-nm excitation.

(C) Green and red fluorescence was measured using mesoscopic imaging through a 6 × 8-mm cranial window in CaMKII α -Cre::NECa mice, with stimulation by a 1-s pulse of white noise. Shown below is an example image of GRAB_{NE2m} fluorescence. The scale bar, 1 mm.

(D) Time course of the change in fluorescence intensity (top) and peak responses (bottom) measured in CaMKII α ::NECa mice and WT mice expressing the NE-insensitive GRAB_{NEmut} sensor (via virus injection at P0–P1; see **STAR Methods**) before and immediately following audio stimulation. Peak response maps from individual mouse and averaged response map were shown. n = 3 animals per group.

(E and F) Schematic illustration (left) of whisker stimulation delivered to CaMKII α ::NECa and GFAP::NECa mice co-expressing both jRGECO1a and GRAB_{NE2m} in excitatory neurons and astrocytes, respectively. Whisker stimuli were applied unilaterally to either the right (top row) or left (bottom row) side, and peak response images, representative traces, and the summary of relative peak $\Delta F/F_0$ measured in CaMKII α ::NECa (middle) and GFAP::NECa (right) mice are shown. The black and gray lines in the schematic illustration (left) indicate the regions of interest (ROIs) used to analyze the representative traces and peak responses. Shown in (F) is the cross-correlation and time lag between the calcium and NE signals measured in response to bilateral whisker stimulation. The n = 5 animals per group.

(G and H) Representative dual-color mesoscopic images (1, top) and traces (1, bottom) of GRAB_{NE2m} and jRGECO1a fluorescence measured in CaMKII α ::NECa (G) and GFAP::NECa (H) mice before, during, and after locomotion. Individual, averaged peak responses, and heatmaps of various cortical regions over time are shown for the GRAB_{NE2m} (2) and jRGECO1a (3) signals. The dashed white lines in (1) indicate the ROIs used to analyze the representative traces. n = 4 animals per group.

(I) Cortex-wide Spearman coefficient measured between the NE and calcium signals in the CaMKII α ::NECa and GFAP::NECa mice (left two images) and between the CaMKII α ::NECa and GFAP::NECa mice for NE and calcium (right two images).

(J) Cross-correlation and time lag between the NE and calcium signals and the onset of locomotion measured in CaMKII α ::NECa (top) and GFAP::NECa (bottom) mice.

Unless noted, summary data are presented as the mean ± SEM. *p < 0.01, *p < 0.05 and n.s., not significant (Student's t test). See also Figures S4 and S5.

- Expression of GRAB_{NE} sensors in cultured cells and *in vivo*
- Fluorescence imaging of HEK293T cells and cultured neurons
- Measurements of spectra
- Tango assay
- Luciferase complementation assay
- Fiber photometry recordings in freely moving mice during optical stimulation
- Fiber photometry recordings in mice during behavioral testing
- Fiber photometry recordings and polysomnographic recordings during the sleep-wake cycle
- Behavioral assays
- Mesoscopic *in vivo* imaging

● QUANTIFICATION AND STATISTICAL ANALYSIS**SUPPLEMENTAL INFORMATION**

Supplemental information can be found online at <https://doi.org/10.1016/j.neuron.2024.03.001>.

ACKNOWLEDGMENTS

This work was supported by the National Key R&D Program of China (2021YFF0502904 to J.F.) and the National Natural Science Foundation of China (31925017 and 31871087 to Y.L.). The study was also supported by grants from the NIH BRAIN Initiative (NINDS U01NS120824 to Y.L.), the Clement and Xinxin Foundation, the Peking-Tsinghua Center for Life Sciences, the State Key Laboratory of Membrane Biology at Peking University School of Life Sciences, and the New Cornerstone Science Foundation through the New Cornerstone Investigator Program and the XPLORE PRIZE (to Y.L.), the Leon Levy Neuroscience Fellowship and NIMH K99MH127295 grants (to J.L.), NIMH/NINDS U01NS113358 and NINDS U01NS103558 (to D.L.), and the Intramural Research Program of the NIH/NIEHS of the United States (1ZIAES103310 to G.C.). We thank Xiaoguang Lei at PKU-CLS and the National Center for Protein Sciences at Peking University in Beijing, China, for their support and assistance with the Opera Phenix high-content screening system and imaging platform. We thank members of the Li lab for helpful suggestions and comments on the manuscript. Some graphics were generated using [BioRender.com](https://biorender.com).

AUTHOR CONTRIBUTIONS

Y.L. supervised the project. J.F. and Y.L. designed the study. J.F. and H.W. performed the experiments related to sensor optimization and characterization in cultured HEK293T cells and neurons with help from G.L. and R.C. J.F. designed and constructed the dual-NECa transgenic mouse line. H.D. and X.M. performed the experiments related to the sleep-wake cycle. J.Z. and G.C. designed and performed the optogenetic stimulation experiments. J.L. and D.L. designed and performed the experiments involving behavior-related recording. J.F. and F.D. designed and performed the mesoscopic imaging experiments with help from H.X. and C.Z. All authors contributed to the data interpretation and data analysis. J.F. and Y.L. wrote the manuscript with input from all other authors.

DECLARATION OF INTERESTS

Y.L. is a member of the journal's advisory board.

Received: June 15, 2023

Revised: January 21, 2024

Accepted: March 1, 2024

Published: March 27, 2024

REFERENCES

1. Berridge, C.W., Schmeichel, B.E., and España, R.A. (2012). Noradrenergic modulation of wakefulness/arousal. *Sleep Med. Rev.* 16, 187–197. <https://doi.org/10.1016/j.smrv.2011.12.003>.
2. Chrousos, G.P. (2009). Stress and disorders of the stress system. *Nat. Rev. Endocrinol.* 5, 374–381. <https://doi.org/10.1038/nrendo.2009.106>.
3. Bast, N., Poustka, L., and Freitag, C.M. (2018). The locus coeruleus-norepinephrine system as pacemaker of attention – a developmental mechanism of derailed attentional function in autism spectrum disorder. *Eur. J. Neurosci.* 47, 115–125. <https://doi.org/10.1111/ejn.13795>.
4. Berridge, C.W., and Waterhouse, B.D. (2003). The locus coeruleus-noradrenergic system: modulation of behavioral state and state-dependent cognitive processes. *Brain Res. Brain Res. Rev.* 42, 33–84. [https://doi.org/10.1016/S0165-0173\(03\)00143-7](https://doi.org/10.1016/S0165-0173(03)00143-7).
5. Brodde, O.-E., Bruck, H., Leineweber, K., and Seyfarth, T. (2001). Presence, distribution and physiological function of adrenergic and muscarinic receptor subtypes in the human heart. *Basic Res. Cardiol.* 96, 528–538. <https://doi.org/10.1007/s003950170003>.
6. Zimmerman, B.G. (1981). Adrenergic facilitation by angiotensin: does it serve a physiological function? *Clin. Sci. (Lond)* 60, 343–348. <https://doi.org/10.1042/cs0600343>.
7. Bito, L., Davson, H., Levin, E., Murray, M., and Snider, N. (1966). The concentrations of free amino acids and other electrolytes in cerebrospinal fluid, *in vivo* dialysate of brain, and blood plasma of the dog. *J. Neurochem.* 13, 1057–1067. <https://doi.org/10.1111/j.1471-4159.1966.tb04265.x>.
8. Justice, J.B. (1993). Quantitative microdialysis of neurotransmitters. *J. Neurosci. Methods* 48, 263–276. [https://doi.org/10.1016/0165-0270\(93\)90097-B](https://doi.org/10.1016/0165-0270(93)90097-B).
9. Watson, C.J., Venton, B.J., and Kennedy, R.T. (2006). *In vivo* measurements of neurotransmitters by microdialysis sampling. *Anal. Chem.* 78, 1391–1399. <https://doi.org/10.1021/ac0693722>.
10. Chefer, V.I., Thompson, A.C., Zapata, A., and Shippenberg, T.S. (2009). Overview of brain microdialysis. *Curr. Protoc. Neurosci.* 47, 7.1.1–7.1.28. <https://doi.org/10.1002/0471142301.ns0701s47>.
11. Lee, G.J., Park, J.H., and Park, H.K. (2008). Microdialysis applications in neuroscience. *Neurol. Res.* 30, 661–668. <https://doi.org/10.1179/174313208X289570>.
12. Olive, M.F., Mehmert, K.K., and Hodge, C.W. (2000). Microdialysis in the mouse nucleus accumbens: a method for detection of monoamine and amino acid neurotransmitters with simultaneous assessment of locomotor activity. *Brain Res. Brain Res. Protoc.* 5, 16–24. [https://doi.org/10.1016/S1385-299X\(99\)00054-9](https://doi.org/10.1016/S1385-299X(99)00054-9).
13. Bruns, D. (2004). Detection of transmitter release with carbon fiber electrodes. *Methods* 33, 312–321. <https://doi.org/10.1016/jymeth.2004.01.004>.
14. Park, J., Kile, B.M., and Wightman, R.M. (2009). *In vivo* voltammetric monitoring of norepinephrine release in the rat ventral bed nucleus of the stria terminalis and anteroventral thalamic nucleus. *Eur. J. Neurosci.* 30, 2121–2133. <https://doi.org/10.1111/j.1460-9568.2009.07005.x>.
15. Robinson, D.L., Hermans, A., Seipel, A.T., and Wightman, R.M. (2008). Monitoring rapid chemical communication in the brain. *Chem. Rev.* 108, 2554–2584. <https://doi.org/10.1021/cr068081q>.
16. Zhou, Z., and Misler, S. (1995). Amperometric detection of stimulus-induced quantal release of catecholamines from cultured superior cervical ganglion neurons. *Proc. Natl. Acad. Sci. USA* 92, 6938–6942. <https://doi.org/10.1073/pnas.92.15.6938>.
17. Muller, A., Joseph, V., Slesinger, P.A., and Kleinfeld, D. (2014). Cell-based reporters reveal *in vivo* dynamics of dopamine and norepinephrine release in murine cortex. *Nat. Methods* 11, 1245–1252. <https://doi.org/10.1038/nmeth.3151>.

18. Nakanishi, J., Takarada, T., Yunoki, S., Kikuchi, Y., and Maeda, M. (2006). FRET-based monitoring of conformational change of the $\beta 2$ adrenergic receptor in living cells. *Biochem. Biophys. Res. Commun.* 343, 1191–1196. <https://doi.org/10.1016/j.bbrc.2006.03.064>.

19. Patriarchi, T., Cho, J.R., Merten, K., Howe, M.W., Marley, A., Xiong, W.H., Folk, R.W., Broussard, G.J., Liang, R., Jang, M.J., et al. (2018). Ultrafast neuronal imaging of dopamine dynamics with designed genetically encoded sensors. *Science* 360, eaat4422. <https://doi.org/10.1126/science.aat4422>.

20. Vilardaga, J.P., Bünnemann, M., Krasel, C., Castro, M., and Lohse, M.J. (2003). Measurement of the millisecond activation switch of G protein-coupled receptors in living cells. *Nat. Biotechnol.* 21, 807–812. <https://doi.org/10.1038/nbt838>.

21. Feng, J., Zhang, C., Lischinsky, J.E., Jing, M., Zhou, J., Wang, H., Zhang, Y., Dong, A., Wu, Z., Wu, H., et al. (2019). A genetically encoded fluorescent sensor for rapid and specific *in vivo* detection of norepinephrine. *Neuron* 102, 745–761.e8. <https://doi.org/10.1016/j.neuron.2019.02.037>.

22. Dana, H., Mohar, B., Sun, Y., Narayan, S., Gordus, A., Hasselman, J.P., Tsegaye, G., Holt, G.T., Hu, A., Walpita, D., et al. (2016). Sensitive red protein calcium indicators for imaging neural activity. *eLife* 5, e12727. <https://doi.org/10.7554/eLife.12727>.

23. Kenakin, T., Watson, C., Muniz-Medina, V., Christopoulos, A., and Novick, S. (2012). A simple method for quantifying functional selectivity and agonist bias. *ACS Chem. Neurosci.* 3, 193–203. <https://doi.org/10.1021/cn200111m>.

24. Meng, C., Zhou, J., Papaneri, A., Peddada, T., Xu, K., and Cui, G. (2018). Spectrally resolved fiber photometry for multi-component analysis of brain circuits. *Neuron* 98, 707–717.e4. <https://doi.org/10.1016/j.neuron.2018.04.012>.

25. Kjaerby, C., Andersen, M., Hauglund, N., Untiet, V., Dall, C., Sigurdsson, B., Ding, F., Feng, J., Li, Y., Weikop, P., et al. (2022). Memory-enhancing properties of sleep depend on the oscillatory amplitude of norepinephrine. *Nat. Neurosci.* 25, 1059–1070. <https://doi.org/10.1038/s41593-022-01102-9>.

26. Osorio-Forero, A., Cardis, R., Vantomme, G., Guillaume-Gentil, A., Katsioudi, G., Devenoges, C., Fernandez, L.M.J., and Lüthi, A. (2021). Noradrenergic circuit control of non-REM sleep substates. *Curr. Biol.* 31, 5009–5023.e7. <https://doi.org/10.1016/j.cub.2021.09.041>.

27. Dong, H., Li, M., Yan, Y., Qian, T., Lin, Y., Ma, X., Vischer, H.F., Liu, C., Li, G., Wang, H., et al. (2023). Genetically encoded sensors for measuring histamine release both *in vitro* and *in vivo*. *Neuron* 111, 1564–1576.e6. <https://doi.org/10.1016/j.neuron.2023.02.024>.

28. Madisen, L., Zwingman, T.A., Sunkin, S.M., Oh, S.W., Zariwala, H.A., Gu, H., Ng, L.L., Palmiter, R.D., Hawrylycz, M.J., Jones, A.R., et al. (2010). A robust and high-throughput Cre reporting and characterization system for the whole mouse brain. *Nat. Neurosci.* 13, 133–140. <https://doi.org/10.1038/nn.2467>.

29. Muzumdar, M.D., Tasic, B., Miyamichi, K., Li, L., and Luo, L. (2007). A global double-fluorescent Cre reporter mouse. *Genesis* 45, 593–605. <https://doi.org/10.1002/dvg.20335>.

30. Madisen, L., Garner, A.R., Shimaoka, D., Chuong, A.S., Klapoetke, N.C., Li, L., van der Bourg, A., Niino, Y., Egolf, L., Monetti, C., et al. (2015). Transgenic mice for intersectional targeting of neural sensors and effectors with high specificity and performance. *Neuron* 85, 942–958. <https://doi.org/10.1016/j.neuron.2015.02.022>.

31. Schwarz, L.A., and Luo, L. (2015). Organization of the locus coeruleus-norepinephrine system. *Curr. Biol.* 25, R1051–R1056. <https://doi.org/10.1016/j.cub.2015.09.039>.

32. Schwarz, L.A., Miyamichi, K., Gao, X.J., Beier, K.T., Weissbourd, B., DeLoach, K.E., Ren, J., Ibanes, S., Malenka, R.C., Kremer, E.J., and Luo, L. (2015). Viral-genetic tracing of the input–output organization of a central noradrenaline circuit. *Nature* 524, 88–92. <https://doi.org/10.1038/nature14600>.

33. Lohani, S., Moberly, A.H., Benisty, H., Landa, B., Jing, M., Li, Y., Higley, M.J., and Cardin, J.A. (2022). Spatiotemporally heterogeneous coordination of cholinergic and neocortical activity. *Nat. Neurosci.* 25, 1706–1713. <https://doi.org/10.1038/s41593-022-01202-6>.

34. Lambert, T.J. (2019). FPbase: a community-editable fluorescent protein database. *Nat. Methods* 16, 277–278. <https://doi.org/10.1038/s41592-019-0352-8>.

35. Kuan, L., Li, Y., Lau, C., Feng, D., Bernard, A., Sunkin, S.M., Zeng, H., Dang, C., Hawrylycz, M., and Ng, L. (2015). Neuroinformatics of the Allen Mouse Brain Connectivity Atlas. *Methods* 73, 4–17. <https://doi.org/10.1016/j.ymeth.2014.12.013>.

36. Kagiampaki, Z., Rohner, V., Kiss, C., Curreli, S., Dieter, A., Wilhelm, M., Harada, M., Duss, S.N., Dernic, J., Bhat, M.A., et al. (2023). Sensitive multi-color indicators for monitoring norepinephrine *in vivo*. *Nat. Methods* 20, 1426–1436. <https://doi.org/10.1038/s41592-023-01959-z>.

37. Barger, Z., Frye, C.G., Liu, D., Dan, Y., and Bouchard, K.E. (2019). Robust, automated sleep scoring by a compact neural network with distributional shift correction. *PLoS One* 14, e0224642. <https://doi.org/10.1371/journal.pone.0224642>.

38. Pnevmatikakis, E.A., and Giovannucci, A. (2017). NoRMCorre: An online algorithm for piecewise rigid motion correction of calcium imaging data. *J. Neurosci. Methods* 291, 83–94. <https://doi.org/10.1016/j.jneumeth.2017.07.031>.

39. Kroeze, W.K., Sassano, M.F., Huang, X.-P., Lansu, K., McCorry, J.D., Giguère, P.M., Sciaiky, N., and Roth, B.L. (2015). PRESTO-Tango as an open-source resource for interrogation of the druggable human GPCRome. *Nat. Struct. Mol. Biol.* 22, 362–369. <https://doi.org/10.1038/nsmb.3014>.

40. Lo, C.A., Kays, I., Emran, F., Lin, T.J., Cvetkovska, V., and Chen, B.E. (2015). Quantification of protein levels in single living cells. *Cell Rep.* 13, 2634–2644. <https://doi.org/10.1016/j.celrep.2015.11.048>.

41. Yizhar, O., Fieno, L.E., Davidson, T.J., Mogri, M., and Deisseroth, K. (2011). Optogenetics in neural systems. *Neuron* 71, 9–34. <https://doi.org/10.1016/j.neuron.2011.06.004>.

42. Hamodi, A.S., Martinez Sabino, A., Fitzgerald, N.D., Moschou, D., and Crair, M.C. (2020). Transverse sinus injections drive robust whole-brain expression of transgenes. *eLife* 9, e53639. <https://doi.org/10.7554/eLife.53639>.

43. Wan, Q., Okashah, N., Inoue, A., Nehmé, R., Carpenter, B., Tate, C.G., and Lambert, N.A. (2018). Mini G protein probes for active G protein-coupled receptors (GPCRs) in live cells. *J. Biol. Chem.* 293, 7466–7473. <https://doi.org/10.1074/jbc.RA118.001975>.

44. Lin, D., Boyle, M.P., Dollar, P., Lee, H., Lein, E.S., Perona, P., and Anderson, D.J. (2011). Functional identification of an aggression locus in the mouse hypothalamus. *Nature* 470, 221–226. <https://doi.org/10.1038/nature09736>.

45. Ma, Y., Shaik, M.A., Kim, S.H., Kozberg, M.G., Thibodeaux, D.N., Zhao, H.T., Yu, H., and Hillman, E.M.C. (2016). Wide-field optical mapping of neural activity and brain haemodynamics: considerations and novel approaches. *Philos. Trans. R. Soc. Lond. B Biol. Sci.* 371, 20150360. <https://doi.org/10.1098/rstb.2015.0360>.

46. Valley, M.T., Moore, M.G., Zhuang, J., Mesa, N., Castelli, D., Sullivan, D., Reimers, M., and Waters, J. (2020). Separation of hemodynamic signals from GCaMP fluorescence measured with wide-field imaging. *J. Neurophysiol.* 123, 356–366. <https://doi.org/10.1152/jn.00304.2019>.

STAR★METHODS

KEY RESOURCES TABLE

REAGENT or RESOURCE	SOURCE	IDENTIFIER
Antibodies		
DAPI fluoromount-G	SouthernBiotech	Cat#0100-20
Bacterial and virus strains		
AAV2/9-hSyn-NE2m (GRAB _{NE2m})	This paper; WZ Biosciences	YL003008-AV9
AAV2/9-hSyn-NE2m (GRAB _{NE2m})	This paper; BrainVTA	PT-2393
AAV2/9-hSyn-NE2h (GRAB _{NE2h})	This paper; WZ Biosciences	YL003011-AV9
AAV2/9-hSyn-NEmut (GRAB _{NEmut})	WZ Biosciences	YL003003-AV9-PUB
AAV2/9-Ef1a-DIO-C1V1-YFP	Gift from Karl Deisseroth	RRID: Addgene_35497
AAV2/9-hSyn-ChrimsonR-tdTomato	Brain Case	BC-0219
AAV2/9-hSyn-NE1m (GRAB _{NE1m})	WZ Biosciences	YL003001-AV9-PUB
AAV2/9-hSyn-Cre	BrainVTA	PT-0136
AAV2/9-hSyn-mApple-CAAX	WZ Biosciences	N/A
Chemicals, peptides, and recombinant proteins		
Norepinephrine bitartrate (NE)	Tocris	Cat#5169
Dopamine hydrochloride (DA)	Sigma-Aldrich	Cat#H8502
Yohimbine hydrochloride (YO)	Tocris	Cat#1127
Epinephrine hydrochloride (Epi)	Sigma-Aldrich	Cat#E4642
Tyramine (TA)	Aladdin	Cat#T105543
Octopamine hydrochloride (OA)	Qualityard	Cat#T0469
Phenethylamine (PEA)	Energy Chemical	Cat#050212
Vanillylmandelic acid (VMA)	MedChemExpress	Cat#HY-113121
Normetanephrine (NMN)	MedChemExpress	Cat#HY-113517
3-methoxy-4-hydroxyphenylglycol (MHPG)	MedChemExpress	Cat#HY-113323
Isoprenaline hydrochloride (ISO)	Sigma-Aldrich	Cat#I5627
ICI 118,551 hydrochloride (ICl)	Sigma-Aldrich	Cat#I127
Acetylcholine chloride (ACh)	Solarbio	Cat#G8320
Serotonin hydrochloride (5-HT)	Tocris	Cat#3547
L-Glutamic acid (Glu)	Sigma-Aldrich	Cat#V900408
γ-aminobutyric acid (GABA)	Tocris	Cat#0344
Adenosine (Ado)	Tocris	Cat#3624
Histamine dihydrochloride (HA)	Tocris	Cat#3545
Desipramine hydrochloride (Desi)	Sigma-Aldrich	Cat#D3900
GBR 12909 (GBR)	Tocris	Cat#0421
Eticlopride hydrochloride (Etic)	Tocris	Cat#1847
Atomoxetine hydrochloride (ATX)	Sigma-Aldrich	Cat#Y0001586
2,2,2-Tribromoethanol (Avetin)	Sigma-Aldrich	Cat#T48402
Isoflurane	RWD Life Science	Cat#R510-22
Experimental models: Cell lines		
HEK293T	ATCC	Cat#CRL-3216; RRID: CVCL_0063
HTLA cells for Tango assay	Gift from Bryan L. Roth	N/A
Experimental models: Organisms/strains		
Rat: wild-type Sprague-Dawley rat pups (P0)	Beijing Vital River Laboratory Animal Technology Co., Ltd.	N/A

(Continued on next page)

Continued

REAGENT or RESOURCE	SOURCE	IDENTIFIER
Mouse: wild-type C57BL/6	Beijing Vital River Laboratory Animal Technology Co., Ltd.	N/A
Mouse: Rosa26-CAG-LSL-jRGECO1a-iP2A-NE2m (dual-NECa)	This paper; Biocytogen Pharmaceuticals Co., Ltd. (Beijing, China)	EGE-XWY-076
Mouse: B6.FVB(Cg)-Tg(Th-cre)Fl172Gsat/Mmucd (TH-Cre)	MMRRC	RRID: MMRRC_031029-UCD
Mouse: B6.Cg-Tg(Camk2a-cre)T29-1Stl/J (CaMKII α -Cre)	The Jackson Laboratory	RRID: IMSR_JAX:005359
Mouse: B6.Cg-Tg(Gfap-cre)77.6Mvs/2J (GFAP-Cre)	The Jackson Laboratory	RRID: IMSR_JAX:024098
Recombinant DNA		
Plasmid: pDisplay vector	Invitrogen	Cat#V66020
Plasmid: pDisplay-NE2m-IRES-mCherry-CAAX	This paper	N/A
Plasmid: pDisplay-NE2h-IRES-mCherry-CAAX	This paper	N/A
Plasmid: pAAV-hSyn-NE2m	This paper	N/A
Plasmid: pAAV-hSyn-NE2h	This paper	N/A
Plasmid: NE2m-SmBit	This paper	N/A
Plasmid: NE2h-SmBit	This paper	N/A
Critical commercial assays		
NanoLuc Luciferase Assay	Promega	Cat#N1110
Software and algorithms		
AccuSleep	Zeke Barger and Charles Frye ³⁷	https://github.com/zekebarger/AccuSleep
Arduino	Arduino.cc	https://www.arduino.cc ; RRID: SCR_017284
ImageJ	NIH	https://imagej.nih.gov/ij/ ; RRID: SCR_003070
MATLAB	MathWorks	https://www.mathworks.com/ ; RRID: SCR_001622
Origin Pro	OriginLab	https://www.originlab.com/ ; RRID: SCR_014212
Spike2	Cambridge Electronic Design Ltd.	https://ced.co.uk/products/spkovic/ ; RRID: SCR_000903
Harmony	Perkin Elmer, Inc.	https://www.perkinelmer.com.cn/ ; RRID: SCR_018809
NoRMCorre	Eftychios A. Pnevmatikakis and Andrea Giovannucci ³⁸	https://github.com/simonsfoundation/NoRMCorre

RESOURCE AVAILABILITY**Lead contact**

Further information and requests for resources and reagents should be directed to and will be fulfilled by the lead contact, Yulong Li (yulongli@pku.edu.cn).

Materials availability

- Plasmids expressing the sensors used in this study have been deposited to Addgene (pDisplay-NE2m-IRES-mCherry-CAAX, #208690; pDisplay-NE2h-IRES-mCherry-CAAX, #208691; pAAV-hsyn-NE2m, #208686; pAAV-hsyn-NE2h, #208687).
- Mouse lines generated in this study have been deposited to Biocytogen Pharmaceuticals Co., Ltd. (Rosa26-CAG-LSL-jRGECO1a-iP2A- GRAB_{NE2m}, dual-NECa, EGE-XWY-076).

Data and code availability

Data and custom programs are available from the [lead contact](#) upon request.

EXPERIMENTAL MODEL AND SUBJECT DETAILS**Cell lines**

HEK293T cells (cat. no. CRL-3216) were obtained from ATCC, cultured, and verified by their morphology and growth curve. The HTLA (an HEK293-derived cell line containing stable integrations of a tTA-dependent luciferase reporter and a β -arrestin2-TEV fusion

gene) cells used in the Tango assay stably express a tTA-dependent luciferase reporter and a β -arrestin2-TEV fusion gene, and were generously provided by Bryan L. Roth.³⁹ All cell lines were cultured at 37°C in DMEM (Gibco) supplemented with 10% fetal bovine serum (Gibco) and 1% penicillin-streptomycin (Gibco) in humidified air containing 5% CO₂.

Primary cell cultures

Postnatal day 0 (P0) Sprague-Dawley rat pups of both sexes, randomly selected from Beijing Vital River, were used to isolate cortical neurons. In brief, the brains were removed, the cortex dissected, neurons were dissociated in 0.25% Trypsin-EDTA (Gibco) was used to dissociate the neurons. The cells were subsequently plated on 12-mm glass coverslips coated with poly-D-lysine (Sigma-Aldrich) and cultured at 37°C in neurobasal medium (Gibco) supplemented with 2% B-27, 1% GlutaMAX, and 1% penicillin-streptomycin (Gibco) in humidified air containing 5% CO₂.

Animals

All animal experiments were performed in accordance with the US National Institutes of Health guidelines for the care and use of laboratory animals, and were approved by the respective Animal Care and Use Committees at Peking University, New York University, and the US National Institute of Environmental Health Sciences. All animals were housed in pairs or as families in a temperature-controlled room with a 12-hour light-dark cycle (lights on from 10 am to 10 pm) with *ad libitum* access to food and water. The *in vivo* experiments were performed on adult (2–12 months of age) mice of both sexes.

Newborn wild-type Sprague-Dawley rat pups (P0) and wild-type C57BL/6 mice (8- to 12-weeks old) were obtained from the Beijing Vital River Laboratory. TH-Cre mice (MMRRC_031029-UCD) were obtained from MMRRC. Rosa26-CAG-LSL-jRGECO1a-iP2A-NE2m (dual-NECa) transgenic mice were generated with help of Biocytogen Pharmaceuticals Co., Ltd. (Beijing, China) as follows. We designed and developed a floxed transgenic mouse line (dual-NECa, EGE-XWY-076) expressing jRGECO1a-iP2A-GRAB_{NE2m} by targeting the Rosa26 locus.³⁰ We first constructed a targeting vector containing the CAG promoter followed by the jRGECO1a and GRAB_{NE2m} coding sequences, separated by an improved P2A self-cleaving peptide⁴⁰ to allow for independent expression of the two proteins. We then used CRISPR/Cas9-mediated homology-directed repair (HDR) to insert the targeting vector into the Rosa26 locus of mouse embryonic stem cells. Successful targeting was confirmed via PCR-based screening and sequencing of the targeted genomic region. Next, the genetically modified embryonic stem cells were injected into eight-cell stage embryos to generate chimeric mice. The chimeric mice were then mated with wild-type mice to obtain germline transmission of the targeted allele. The resulting dual-NECa transgenic mouse line stably expressed both the green fluorescent GRAB_{NE2m} sensor and the red calcium indicator jRGECO1a under the control of the CAG promoter at the Rosa26 locus upon excision of the floxed stop cassette by Cre recombinase. CaMKII α -Cre (005359; JAX) and GFAP-Cre (024098; JAX) were used in this study to further drive the expression of GRAB_{NE2m} and jRGECO1a.

METHOD DETAILS

Molecular cloning

In this study, the molecular clones were generated using Gibson assembly. The DNA fragments were amplified with primers containing 25–30-bp overlap. Sanger sequencing was used to confirm the sequence of all clones. The pDisplay vector with an upstream IgK leader sequence and a downstream IRES-mCherry-CAAX cassette was used to clone all cDNAs encoding the GRAB_{NE} sensors, providing cell membrane targeting and labeling. For sensor optimization, amino acids were randomly mutated using PCR amplification with NNB codons at the target sites. The pAAV vector containing the human *Synapsin* promoter was used to express the GRAB_{NE} sensors or GRAB_{NEmut} in neurons. For luciferase complementation assay, the GRAB_{NE2m}-SmBit and GRAB_{NE2h}-SmBit constructs were modified from β 2AR-SmBit, and the LgBit-mGsi was a gift from Nevin A. Lambert.

Expression of GRAB_{NE} sensors in cultured cells and *in vivo*

GRAB_{NE} sensors were expressed in HEK293T cells and cultured rat cortical neurons as previously reported.²¹

For *in vivo* virus-mediated expression, adult mice were anesthetized with either an i.p. injection of 2,2,2-tribromoethanol (Avertin, 500 mg/kg body weight, Sigma-Aldrich) or 1.5% isoflurane by inhalation, 2% lidocaine hydrochloride was injected subcutaneously under the scalp. the mice were then placed in a stereotaxic frame (RWD Life Science). Small craniotomy holes were prepared in the skull for virus injection.

In Figures 2A–2E, AAVs expressing hSyn-GRAB_{NE2m/NE2h} and Ef1a-DIO-C1V1-YFP⁴¹ (Vigene, 1 \times 10¹³ titer genomic copies per ml) were injected into the LC (AP: -5.45 mm relative to Bregma; ML: \pm 1.25 mm relative to Bregma; DV: 2.25 mm below the dura) of TH-Cre mice at a rate of 100 nl/min and in a volume of 500 nl. Four weeks after virus injection, we implanted multi-mode optical fiber probes (105/125 μ m core/cladding) into the LC (AP: -5.45 mm relative to Bregma; ML: \pm 0.85 mm relative to Bregma; DV: 3.5 mm below the dura). In Figures 2F–2H, AAVs that express GRAB_{NE2m} were injected into the mPFC (AP: +1.9 mm relative to bregma; ML: \pm 0.3 mm relative to bregma; and DV: -1.9 from the dura) of wild-type C57BL/6 mice. AAVs expressing hSyn-ChrimsonR-tdTomato were injected into either the VTA (AP: -2.9 mm relative to bregma; ML: \pm 0.65 mm relative to bregma; and DV: -4.1 mm from the dura) or the LC (AP: -5.3 mm relative to bregma; ML: \pm 0.9 mm relative to bregma; and DV: -2.5 mm from the dura) on

the same side of the GRAB_{NE2m} injection site. The injection was performed at a rate of 50 nl/min, with a total volume of 300 nl. An optical fiber (200- μ m diameter, 0.37 NA; Inper) was then implanted 0.1 mm above the injection site.

In Figure 3, AAVs expressing GRAB_{NE1m}, GRAB_{NE2m}, and GRAB_{NE2h} (Vigene, 1 \times 10¹³ titer genomic copies per ml) were unilaterally injected into the lateral hypothalamus (AP: -1.7 mm relative to Bregma; ML: +0.90 mm relative to Bregma; DV: 6.05 mm below the dura) of wild-type C57BL/6 mice at a rate of 10 nl/min and in a volume of 100 nl. A 400- μ m optic fiber (Thorlabs, BFH48-400) housed in a ceramic ferrule (Thorlabs, SFLC440-10) was implanted 0.2 mm above the injection site. The experiments were performed three weeks after virus injection.

For experiments in Figure 4, a fine glass pipette and a micro-syringe pump (Nanoliter 2010 injector, World Precision Instruments) were used to microinject approximately 300 nl of AAV9-hSyn-NE2m (Vigene, 1 \times 10¹³ titer genomic copies per ml) or AAV9-hSyn-Cre virus (BrainVTA, 3 \times 10¹² titer genomic copies per ml) into the mPFC (AP: +1.9 mm relative to Bregma, ML: -0.3 mm relative to Bregma, DV: 1.9 mm below the dura) and/or POA (AP: 0 mm relative to Bregma, ML: -0.6 mm relative to Bregma, DV: 4.9 mm below the dura) at a rate of 30 nl/min.

For experiments in Figure 5, we crossed homozygous of the floxed dual-NECa transgenic mice with CaMKII α -Cre (005359; JAX) or GFAP-Cre (024098; JAX) to obtain CaMKII α ::NECa and GFAP::NECa offspring, respectively. To achieve widespread expression of GRAB_{NEmut} through the entire cortex, we utilized a method previously described⁴² in which 4 μ l of AAV9-hSyn-NEmut virus (Vigene, 1 \times 10¹³ titer genomic copies per ml) was bilaterally injected into the transverse sinus of P0–P1 C57BL/6 mouse pups at a rate of 1.2 μ l/min.

Fluorescence imaging of HEK293T cells and cultured neurons

To visualize cells expressing GRAB_{NE} sensors, we used either an inverted Ti-E A1 confocal microscope (Nikon) equipped with a 10x/0.45 NA (numerical aperture) objective, a 20x/0.75 NA objective, a 40x/1.35 NA oil-immersion objective, a 488-nm laser, and a 561-nm laser or an Opera Phenix high-content screening system (PerkinElmer) equipped with a 20x/0.4 NA objective, a 40x/1.1 NA water-immersion objective, a 488-nm laser, and a 561-nm laser. For confocal microscopy, the GFP signal was collected using a 525/50-nm emission filter combined with the 488-nm laser, while the RFP signal was collected using a 595/50-nm emission filter combined with the 561-nm laser. For the Opera Phenix system, the GFP and RFP signals were collected using a 525/50-nm and 600/30-nm emission filter, respectively. To calibrate the fluorescence signal produced by the green fluorescent GRAB_{NE} sensors, we used the GFP/RFP ratio. The dose-dependent response and on and off kinetics were determined as previously described.²¹

Measurements of spectra

HEK293T cells expressing GRAB_{NE2m} or GRAB_{NE2h} were harvested and transferred to a 384-well plate. Excitation and emission spectra were measured at 5-nm increments with a 20-nm bandwidth using a Safire2 multi-mode plate reader (TECAN) in the presence or absence of 10 μ M NE. Control cells not expressing a sensor were used to obtain background fluorescence for subtraction.

Tango assay

HTLA cells expressing the wild-type α 2AR, GRAB_{NE2m}, or GRAB_{NE2h} were exposed to varying concentrations of NE (ranging from 0.1 nM to 10 μ M) and cultured for 12 h to allow luciferase gene expression. Luminescence was then measured using a VICTOR X5 multilabel plate reader (PerkinElmer) after adding Furimazine (NanoLuc Luciferase Assay, Promega) to a final concentration of 5 mM.

Luciferase complementation assay

The luciferase complementation assay was performed as described previously.⁴³ Forty-eight hours after transfection, the cells were washed with phosphate-buffered saline and transferred to opaque 96-well plates containing diluted NE solutions ranging from 1 nM to 100 μ M. Luminescence was measured using NLuc after adding Furimazine (NanoLuc Luciferase Assay, Promega) to each well.

Fiber photometry recordings in freely moving mice during optical stimulation

In Figure 2, fiber photometry recording in the LC was performed using a 473-nm laser, which produced an output power of 25 μ W at the end of the fiber. The resulting emission spectra were analyzed using a linear unmixing algorithm (<https://www.niehs.nih.gov/research/atniehs/labs/ln/pi/iv/tools/index.cfm>). The coefficients from the unmixing algorithm represent the fluorescence intensities of various fluorophores.²⁴ To evoke C1V1-mediated NE release, pulse trains (10-ms pulses at 20 Hz for 1 s) were delivered to the LC using a 561-nm laser with an output power of 9.9 mW at the end of the fiber. To induce ChrimsonR-mediated NE release, a 635-nm laser (1–300 mW, LL-Laser) was used for optogenetic stimulation, with the light power at the tip of the fiber set at 10 mW. Optical stimulation was delivered at 20 Hz (1-s duration for LC, 5-s duration for VTA) simultaneously with photometry recording.

Fiber photometry recordings in mice during behavioral testing

For the fiber photometry recordings in Figure 3, GRAB_{NE} sensors were excited using a 400-Hz sinusoidal blue LED light (30 mW; M470F1 driven by an LED1B driver; both from Thorlabs), which was bandpass filtered (passing band: 472 \pm 15 nm, Semrock, FF02-472/30-25) and transmitted to the brain. The emission light traveled back through the same optic fiber, through a bandpass filter (passing band: 534 \pm 25 nm, Semrock, FF01-535/50), and was recorded using a Femtowatt Silicon Photoreceiver connected

to an RZ5 real-time processor (Tucker-Davis Technologies). A custom-written program was used to extract the 400-Hz signals in real time and determine the intensity of the GRAB_{NE} fluorescence signal.

All behavioral tests were performed at least 1 hour after the onset of the dark cycle. For the tail suspension test, each mouse was lifted gently off the bottom of its cage six times for 60 s each, with a minimum of 1 min between each lift. In the forced swimming test, the mouse was gently placed in a 1000-ml conical flask filled with lukewarm water and then removed after 4-6 min. The mouse was then gently dried with paper towels and placed on a heating pad inside its home cage. No aggressive behavior was observed during the test. All videos were recorded at 25 frames per second and manually annotated frame-by-frame using a custom MATLAB program (MathWorks).⁴⁴

Fiber photometry recordings and polysomnographic recordings during the sleep-wake cycle

To measure the fluorescence signals in Figure 4, a 200-μm optical fiber cannula (Fiber core: 200 μm; numerical aperture: 0.37; Inper, Zhejiang, China) was implanted 0.1 mm above the virus injection site and fixed to the skull using dental cement.

To monitor the animal's sleep-wake state, EEG electrodes were implanted into the craniotomy holes above the frontal cortex and visual cortex, and EMG wires were placed in the trapezius muscles on both sides. The electrodes were connected to a microconnector and fixed to the skull using dental cement. The microconnector was connected via a flexible cable and attached to an electric slip ring, allowing the mouse to move freely. The cortical EEG and neck EMG signals were amplified (NL104A, Digitimer), filtered (NL125/6, Digitimer), digitized using a Power1401 digitizer (Cambridge Electronic Design Ltd.), and recorded using Spike2 software (Cambridge Electronic Design Ltd.) at a sampling rate of 1000 Hz.

A fiber photometry system (Thinker Tech, Nanjing, China) was used to record the fluorescence signals in freely moving mice. Blue (473-nm) and yellow (580-nm) LED lights (Cree LED) were bandpass filtered (470/25 nm, model 65-144 and 572/28 nm, model 84100, Edmund Optics), reflected by a 495-nm long-pass dichroic mirror (model 67-069, Edmund Optics) and a multi-band filter (model 87-282, Edmund Optics) dichroic mirror, and then focused using a 20x objective lens (Olympus). An optical fiber guided the light between the commutator and the implanted optical fiber cannula. The excitation light power at the tip of the optical fiber was adjusted to 20–30 μW in order to minimize photobleaching and was delivered at 100 Hz with a 5-ms pulse duration. Green fluorescence was bandpass filtered (525/39 nm, model MF525-39, Thorlabs), red fluorescence was bandpass filtered (615/20 nm, model 87753, Edmund Optics), and the resulting emissions were collected using a photomultiplier tube (model H10721-210, Hamamatsu). The current output from the photomultiplier tube was converted to a voltage signal using an amplifier (model C7319, Hamamatsu) and passed through a low-pass filter. The analog voltage signals were then digitized using an acquisition card (National Instruments). Photometry signals and polysomnographic recordings were aligned based on a TTL signal. To minimize autofluorescence of the optical fiber, the recording fiber was photobleached using a high-power LED before recording. Background autofluorescence was subtracted from the recorded signals during subsequent analysis.

Behavioral assays

CaMKIIα::NECa, GFAP::NECa, floxed dual-NECa, and wild-type C57BL/6 mice (8- to 12-weeks old) of both sexes were subjected to open-field test and elevated plus maze test. Mice were handled for 3 days for 3 min each day before experiments. The behavior assays were blindly analyzed. The open-field test was performed in ENV-510 test chambers (27.3 cm x 27.3 cm x 20.3 cm, Med Associates) with smooth interior walls. The center area of the open field was defined as a 14.29 cm x 14.29 cm zone centered in the arena. At the start of the test, mice were placed in one of four corners of the arena. Locomotion traces were recorded by infrared photo beams for 10 min for each mouse. Time and distance in the center area and total distance were analyzed by the Activity Monitor 7 software (Med Associates). The elevated plus maze test was performed in an elevated plus maze equipped with two opposite open arms without walls (30 cm x 6 cm), two opposite closed arms (30 cm x 6 cm x 15 cm) and a central platform (5 cm x 5 cm). The maze was elevated 80 cm above the floor. At the start of the test, mice were first placed in the center zone facing one of the open arms. Mice were allowed to explore the maze for 10 min. Locomotion traces were recorded by an infrared video camera. The time, distance, and entries were quantified and analyzed by Panlab 3.0 software (Harvard Apparatus).

Mesoscopic *in vivo* imaging

The surgery to prepare the imaging window and implant the EMG electrodes was performed on CaMKIIα::NECa, GFAP::NECa, or wildtype mice expressing GRAB_{NEmut}. Anesthesia was induced with an i.p. injection of 2,2,2-tribromoethanol (Avertin, 500 mg per kg) and maintained with 1% isoflurane. The mouse was then fixed in a stereotaxic frame, and 2% lidocaine hydrochloride was injected under the scalp. To protect the corneas, erythromycin ophthalmic ointment was applied to both eyes. The scalp and underlying muscles were carefully removed to expose the skull, and the majority of the skull above the dorsal cortex was replaced with a custom-made coverslip to create an optical window. EMG electrodes were implanted as described above, and the mice were given at least 7 days to recover, followed by an additional 3 days to habituate to the head fixation before imaging.

Mesoscopic imaging was performed using a customized dual-color microscope equipped with a 2x/0.5 NA objective lens (Olympus, MVPLAPO2XC), two 1x/0.25 NA tube lenses (Olympus, MVPLAPO1X), and two sCMOS cameras (Andor, Zyla 4.2 Plus, 2,048x2,048 pixels, 16-bit). A multi-line fiber-coupled laser system (Changchun New Industries Optoelectronics Tech. Co., Ltd., RGB-405/488/561/642nm-220mW-CC32594) generated three excitation wavelengths (405 nm, 488 nm, and 561 nm). Emission light was passed through a long-pass dichroic mirror (Thorlabs, DMLP567L) and either a 525/36-nm or 609/34-nm emission filter (Chroma)

and captured by the sCMOS cameras. Both the excitation laser and the camera exposure were triggered by an Arduino board (Uno) using custom-written programs. Dual-color imaging was performed using alternating illumination between the 405-nm laser and the 488-nm or/and 561-nm laser. Images were acquired using Micro-Manager 2.0 at 512×512-pixel resolution at a rate of 5 Hz with 40-ms exposure.

During imaging, the mice were head-fixed but could run freely on a linear treadmill. A near-infrared camera with an infrared LED was used to record the mouse's behavior and pupil size. For auditory stimulation, 1 s of 70-dB white noise was generated using a RZ6 Multi I/O Processor (Tucker-Davis Technologies) and delivered via a magnetic speaker. For whisker stimulation, a 1-s pendular stick was delivered to the mouse whisker either unilaterally or bilaterally. For visual stimulation, 50-ms of a flashing LED light was delivered to the mouse eye either unilaterally or bilaterally. Locomotion activity was recorded using the encoder in the treadmill.

QUANTIFICATION AND STATISTICAL ANALYSIS

For the imaging experiments using cultured HEK293T cells and primary neurons, fluorescence intensity was first quantified using ImageJ software (National Institutes of Health) or Harmony software (PerkinElmer, Inc.) for and then analyzed using a custom-written MATLAB script (MathWorks) or Origin Pro (OriginLab).

The photometry data were analyzed using a custom program written in MATLAB. To calculate $\Delta F/F_0$, baseline values were measured during REM sleep with no apparent fluctuations. To compare the change in fluorescence between animals, the z-score-transformed $\Delta F/F_0$ was normalized using the standard deviation of the baseline signals.

EEG and EMG recordings were used to determine the animal's sleep-wake state. In brief, the EEG and EMG data were filtered at 0.5–100 Hz and 30–500 Hz, respectively, and semi-automatically scored off-line in 4-s epochs of wakefulness, REM sleep, and NREM sleep using AccuSleep (<https://github.com/zekebarger/AccuSleep>)³⁷; the defined sleep-wake states were confirmed by visual examination and corrected if necessary. Wakefulness was defined as desynchronized low-amplitude EEG activity and high-amplitude EMG activity with phasic bursts. NREM sleep was defined as synchronized EEG activity with high-amplitude delta rhythm (0.5–4 Hz) and low EMG activity. REM sleep was defined as a pronounced theta rhythm (6–10 Hz) and low EMG activity. EEG spectral analysis was estimated using a short-time fast Fourier transform (FFT).

To characterize NE transients during NREM sleep. To better demonstrate NE oscillations, micro-arousals (<30 seconds) was masked. First, we smooth the signal using a low-pass filter (Matlab *butter* function). Then, the NE peaks was selected by Matlab *findpeaks* function (minimum peak prominence of 2 z-score). NE and calcium transients were aligned according to the peak of NE. Peaks and full width at half maximum (FWHM) were obtained by the Matlab *findpeaks* function. The transient interval of NE was the difference between the times of adjacent peaks. The histogram of peak, FWHM and interval of NE signals were plotted by Origin.

For the mesoscopic imaging data, raw images acquired from each camera were calibrated to ensure uniformity across the imaging region, and movement-related artifacts were corrected using the motion-correction algorithm NoRMCorre.³⁸ The corrected image stack with a size of 512 × 512 pixels was downsampled by a factor of 0.5 to 256 × 256 pixels for further analysis. For dual-color imaging, the red-channel images were registered to the green-channel images by performing an automated transformation using the "similarity" mode of the MATLAB function "imregtform". The same transformation was then applied to all red-channel images to align them with their corresponding green-channel images. The resulting image stack was saved as a binary file to facilitate the input and output of large files. A mask was created to exclude background and blood vessel pixels from the corrected image stack using the machine learning-based ImageJ plugin Trainable Weka Segmentation (v3.3.2); these minimized artifacts caused by blood vessel constriction and dilation. To correct the effects of hemodynamics on fluorescence,^{33,45,46} we performed a pixel-by-pixel correction based on a linear regression of the ligand-dependent signals (excited by 488-nm or 561-nm light) against the ligand-independent signals (excited by 405-nm light) for both GRAB_{NE2m} and jRGECO1a based on their respective spectra.

Baseline images were smoothed using a Gaussian filter ($\sigma = 2$), and linear regression was performed for each pixel by regressing the baseline fluorescence intensity of the 405-nm-excited channel onto the 488-nm or 561-nm signal. The regression coefficient was then used to rescale the 405-nm channel, which was then subtracted from the 488-nm or 561-nm signal. The corrected signal was added to the averaged rescaled 405-nm channel signal to avoid negative values. The response of each pixel was calculated using the following equation: $\Delta F/F_0 = (F - F_0) / F_0$, where F_0 is defined as the average baseline fluorescence intensity.

We registered the mean fluorescence image to a 2D projection of the Allen Common Coordinate Framework v3 (CCFv3) using four manually identified anatomical landmarks, including the left, center, and right points in the boundary between the anterior cortex and the olfactory bulbs, and the medial point at the base of the retrosplenial cortex. To analyze the time course of the response in a specific brain region, we calculated the average $\Delta F/F_0$ value for all available pixels within that region. To align and average the responses across the entire cortex from multiple mice, we developed a custom script to first register the peak response image for each individual mouse to the Allen CCFv3 and then averaged the images, preserving only the intersection pixels.